

# 3D Image Processing for Assistance in Localizing the Deep Cerebral Structures

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*EPIDAURE Project*  
*INRIA Sophia Antipolis - France*

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## Research agreement no 97506

### Improvement of Target Determination for Deep Brain Stimulation by Registration of MR Images with a Functional Atlas of the Basal Ganglia

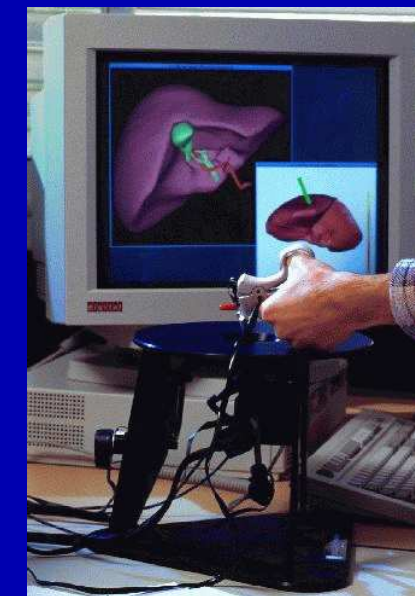
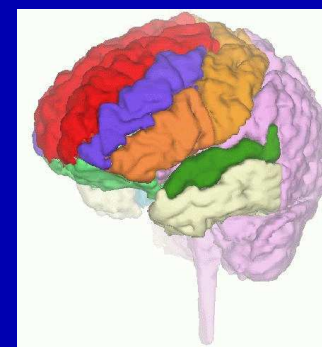
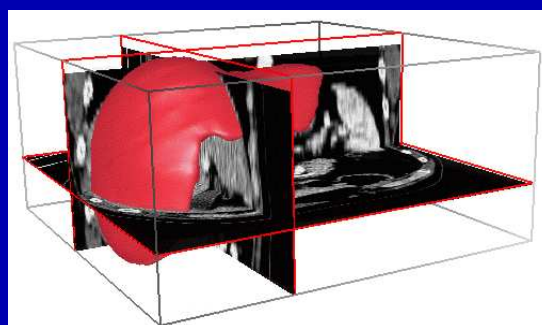
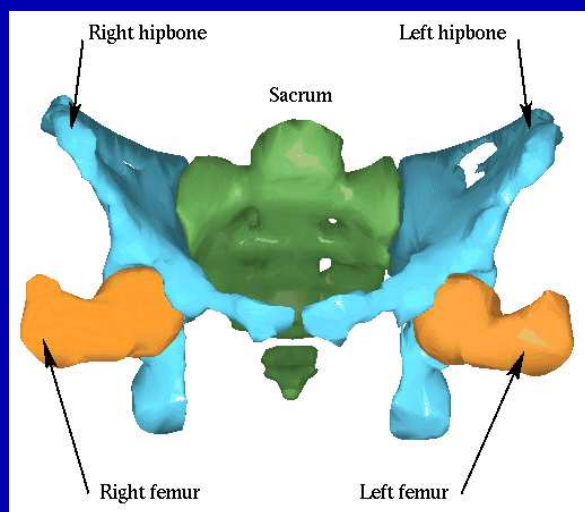
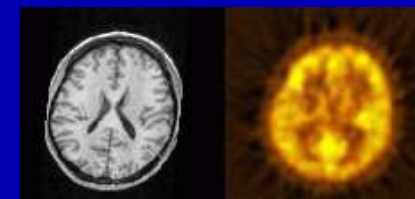
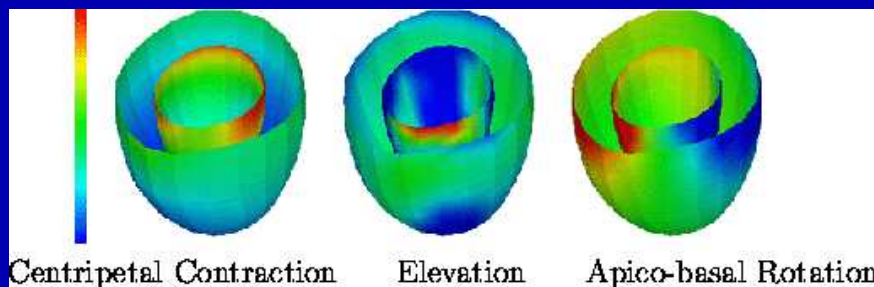
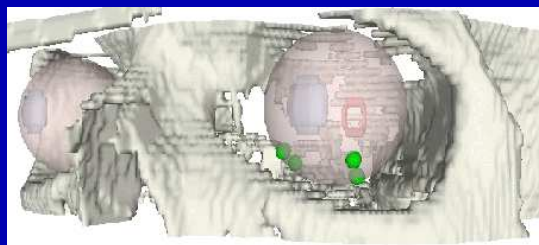
- Medtronic - Bakken Research Center B.V.  
Maastricht - The Netherlands
- INSERM U289 - Institut National de la Santé et de la Recherche Médicale  
Service de Neuroradiologie - Centre d'Investigation Clinique  
Hôpital de la Salpêtrière, Paris - France
- INRIA - Institut National de la Recherche en Informatique et en Automatique  
EPIDAURE Project  
Sophia Antipolis - France

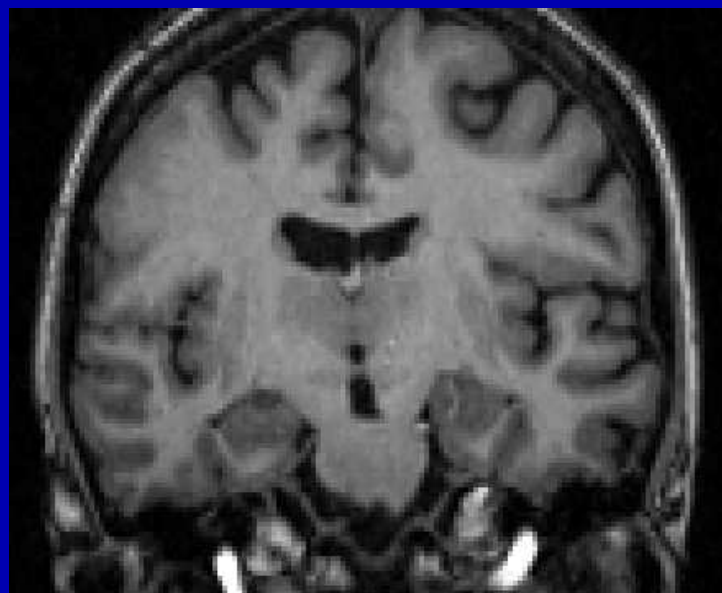
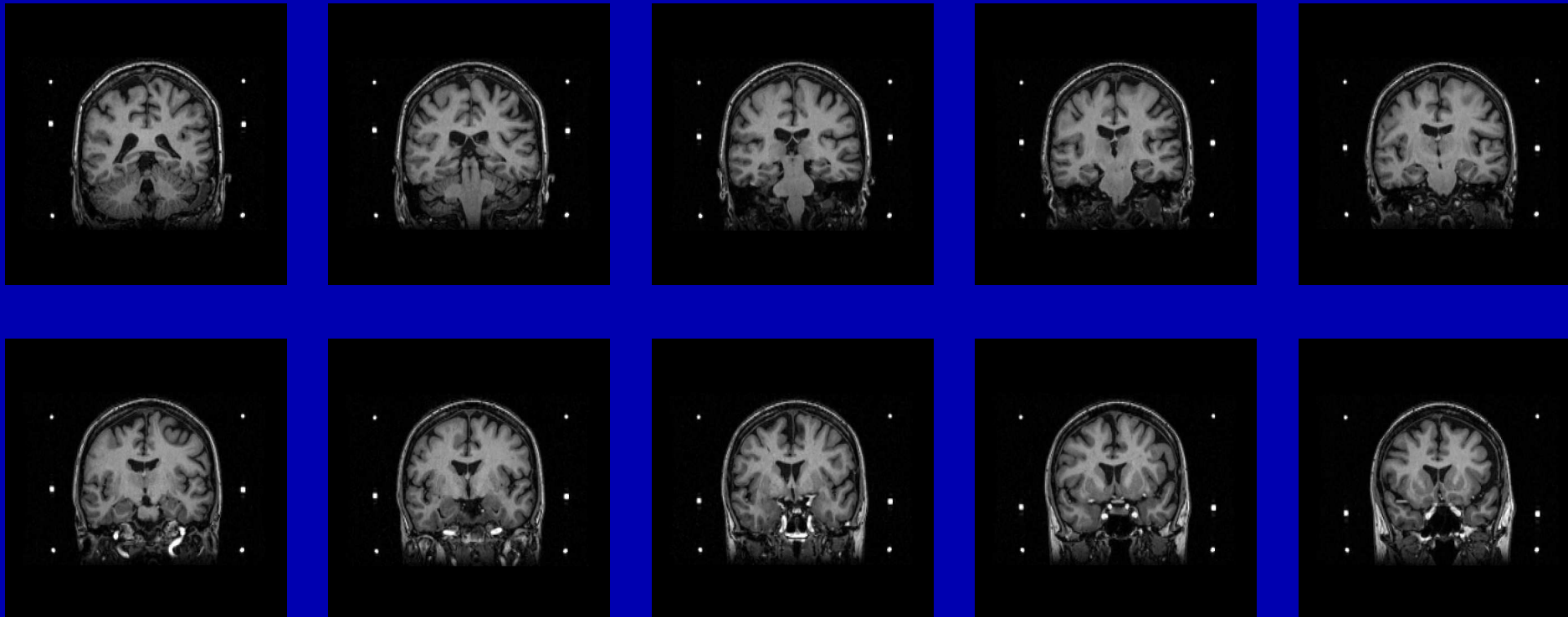
The objective of the EPIDAURE Project is to design and develop tools for the computer analysis of multidimensional, multimodal medical images (CT, MR, US, nuclear medicine).

Headed by Prof. Nicholas Ayache, 20 people (6 senior researchers, 10 Ph.D. students).

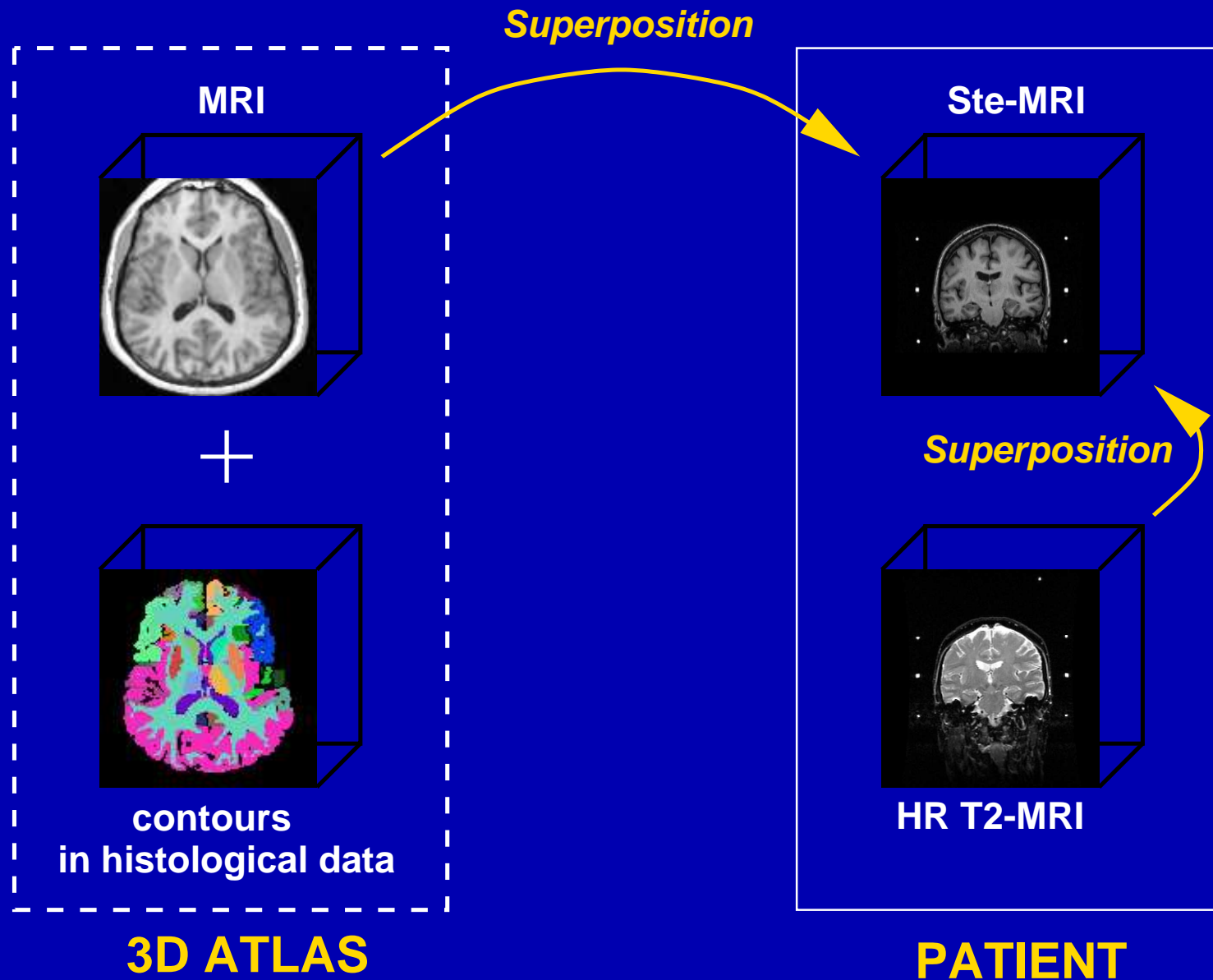
4 European Community Projects (video-surgery simulation, brain morphometry for MS and SC, analysis of CJD in MR images, 3D-US guided manipulator for neurosurgery).

Numerous industrial (Focus Imaging, GEMS, Nycomed, Medtronic, Philips, Sanofi, ...) and medical (Boston, Edinburgh, Liverpool, Leuven, London, Nice, Paris, Strasbourg hospitals) collaborations.



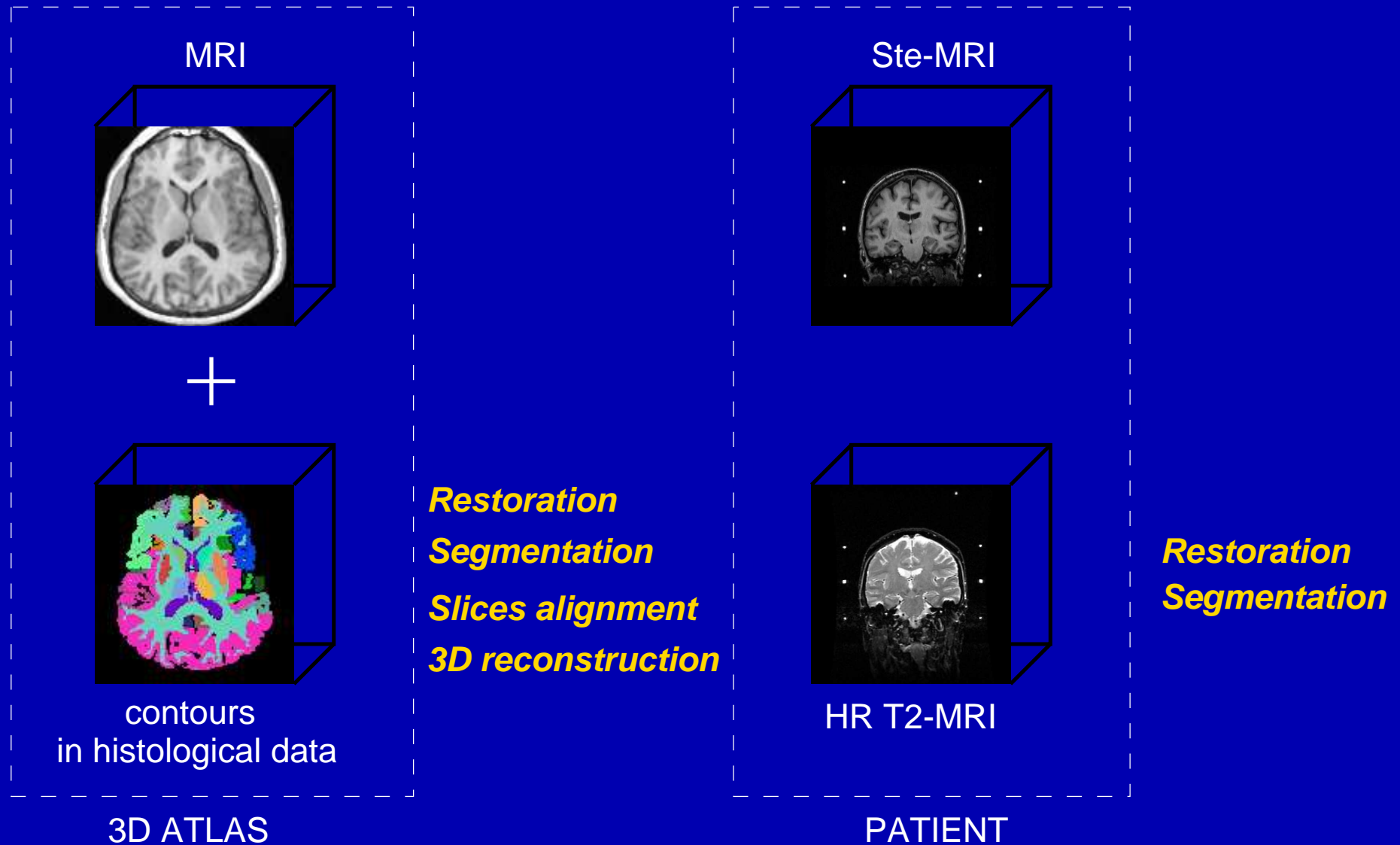


**How to localize accurately the deep cerebral structures that are not clearly visible in the stereotactic MR image?**



► Adapt and develop 3D image processing algorithms for assisting the localization

# 1. Preprocessing of data

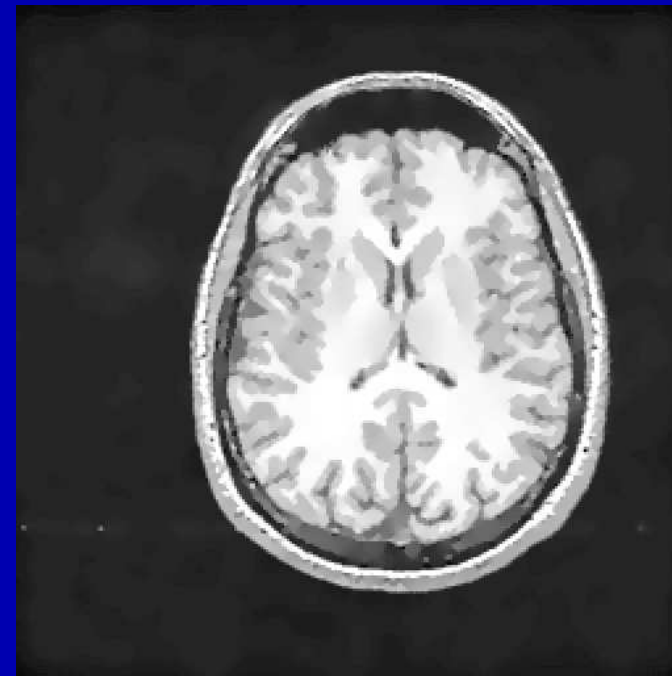
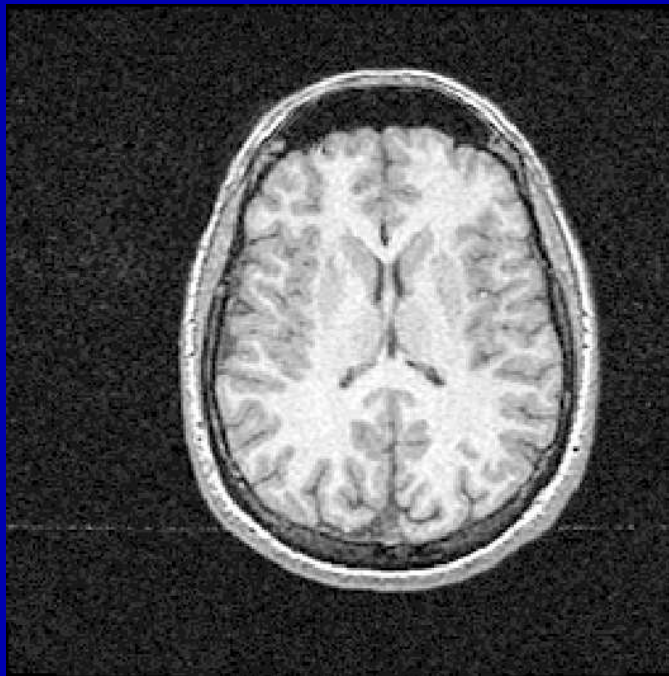


## Processing of MR data: restoration of images

MR images can be corrupted by noise or a non-homogeneous multiplicative bias.

Deep structures are difficult to perceive, especially in 3D.

- ▶ Smoothing the image in 3D yet preserving important intensity discontinuities

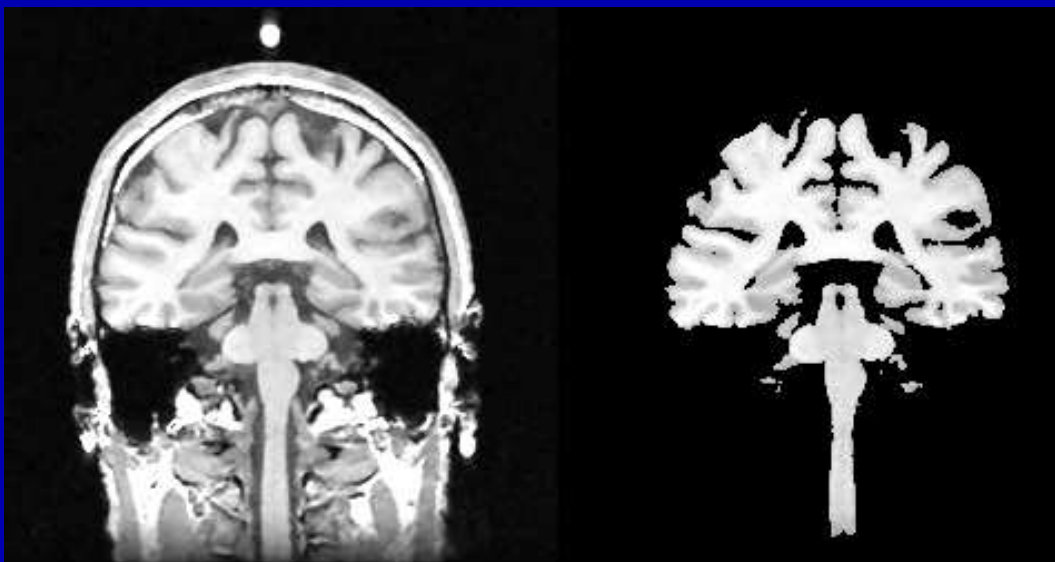


*Non-isotropic diffusion applied to a MR image*

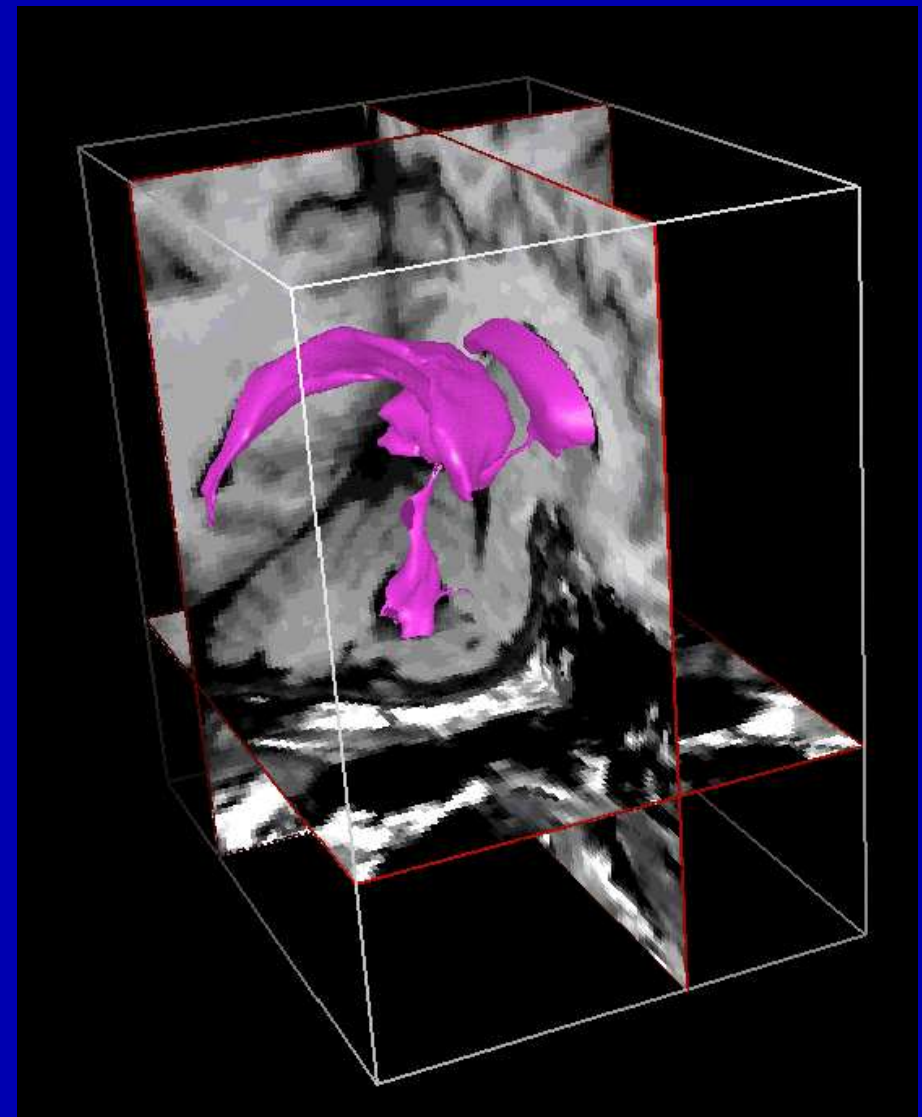
## Processing of MR data: segmentation of structures

Difficult to take into account the 3D consistency.

► Need for a 3D tool



*Automatic segmentation of the cortical boundary*



*A deformable surface eases the segmentation of cerebral ventricles*



## Construction of a 3D atlas: restoration of histological slices

Images can be corrupted by artifacts or noise.

Some structures can be difficult to perceive.

► Smoothing the image yet preserving important intensity discontinuities



*Non-isotropic diffusion applied to a rat's brain histological slice*

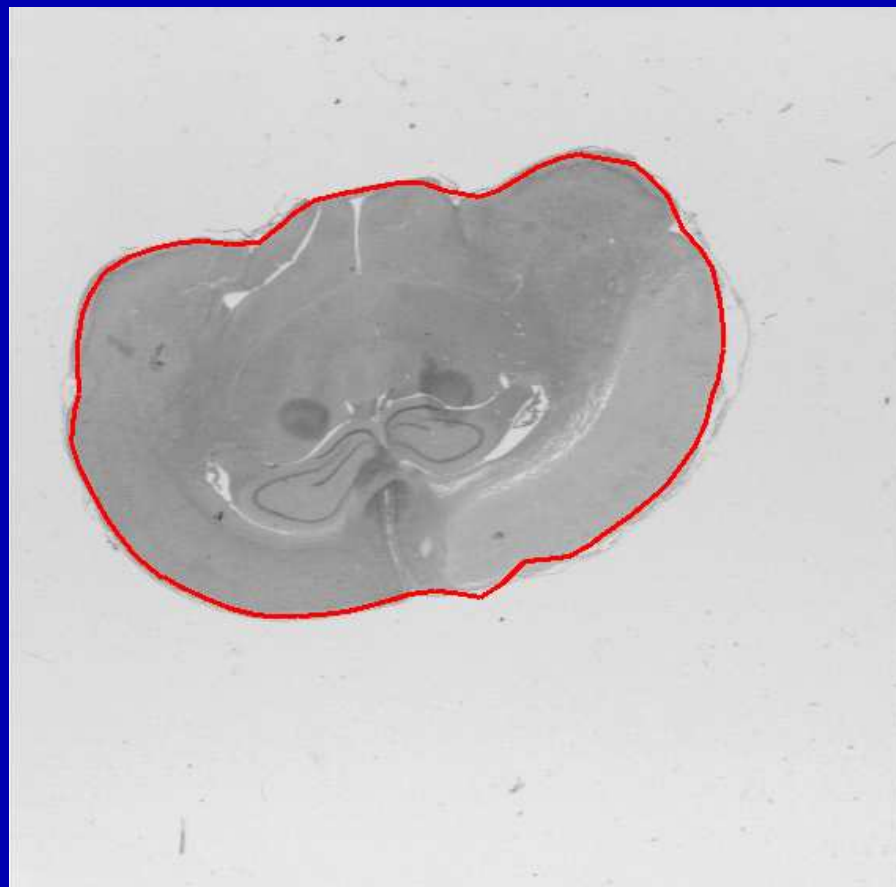
## Construction of a 3D atlas: segmentation of structures

Delineating structures needs high anatomy knowledge.

Tedious task.

Difficult to achieve the pixel resolution.

► **Need for a user-guided tool**

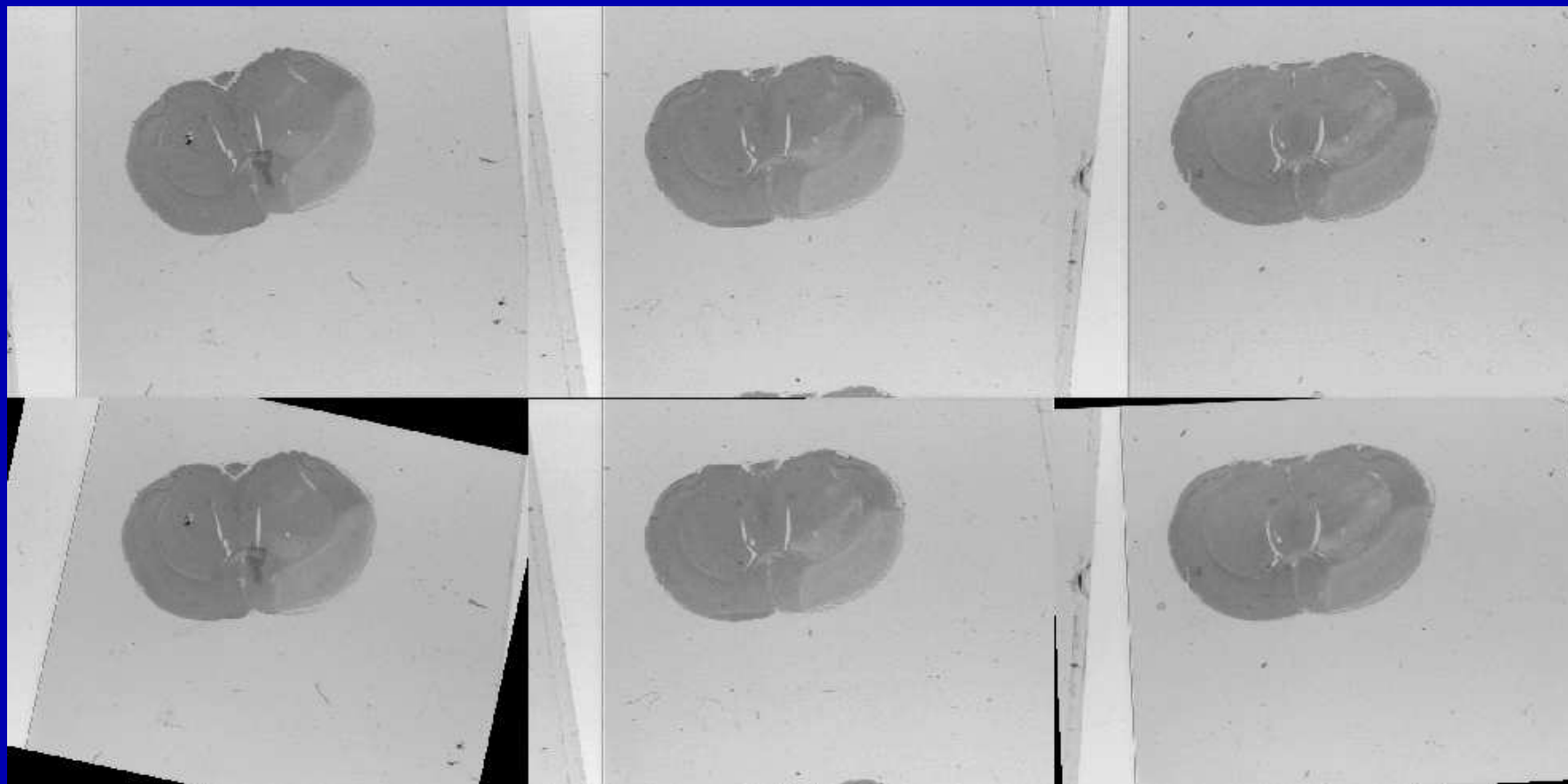


*A deformable contour (in red) eases the segmentation in a rat's brain histological slice*

## Construction of a 3D atlas: alignment of slices

Images of histological slices can be shifted during the acquisition process.  
Manual or fiducial-based alignment may be not accurate enough .

### ► Aligning automatically the slices

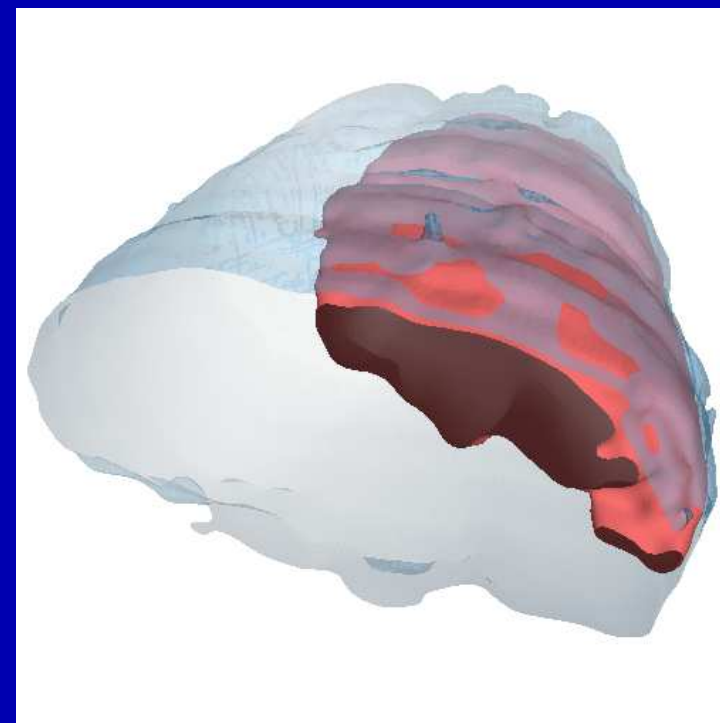
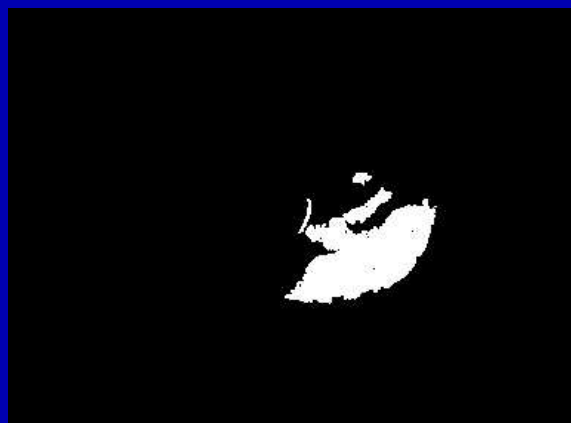
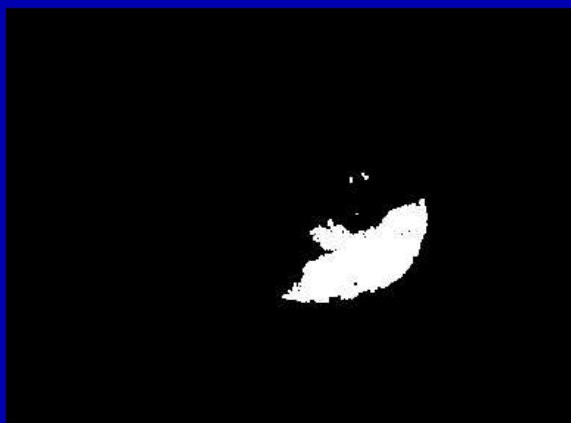
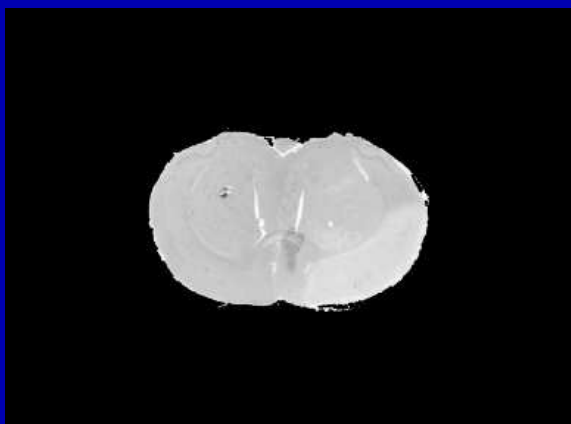


*Automatic alignment of three successive rat's brain histological slices*

## Construction of a 3D atlas: 3D reconstruction

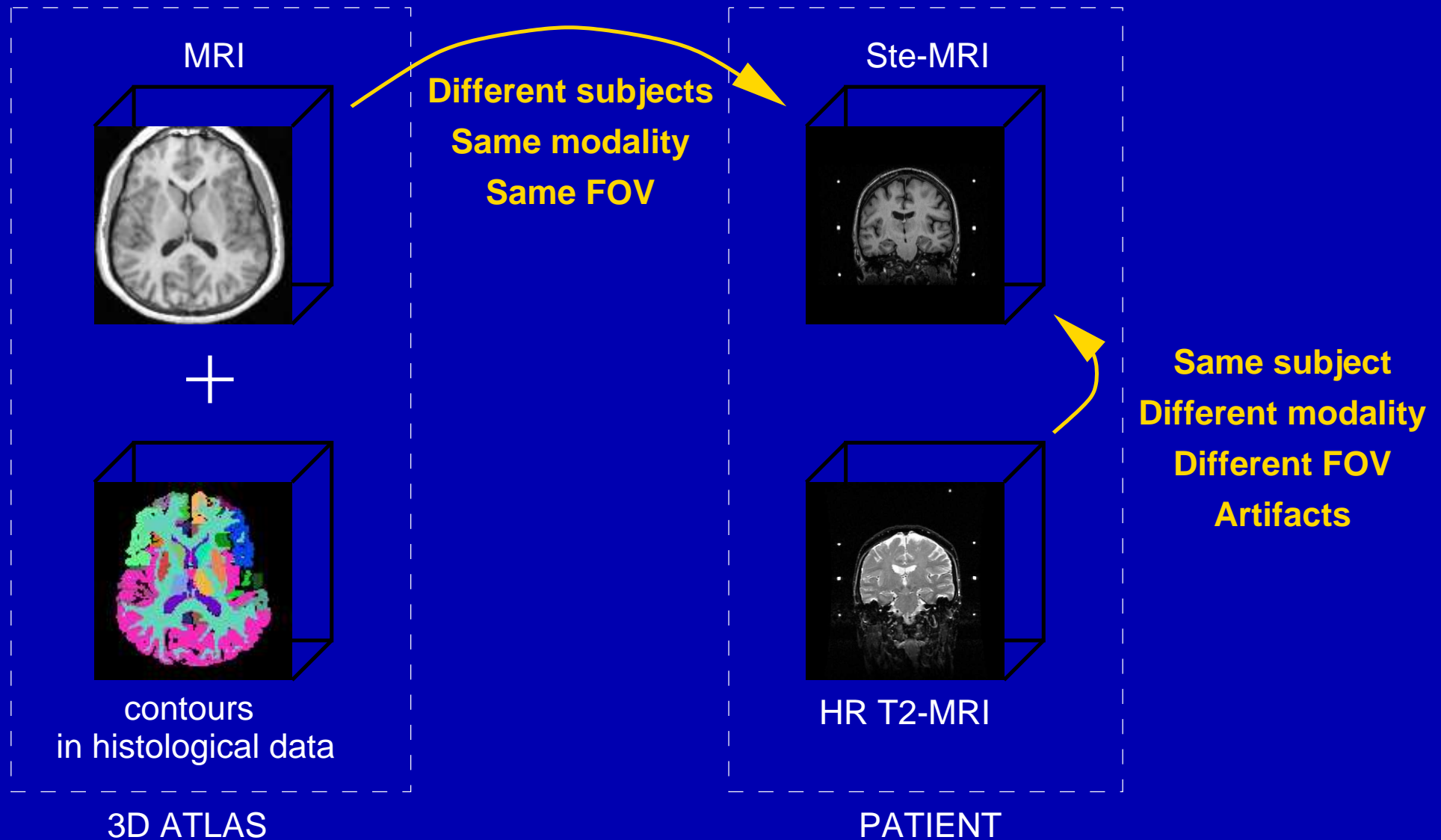
Once the slices are segmented and aligned:

- ▶ The 3D surface reconstruction allows us to visualize the structures from any point of view

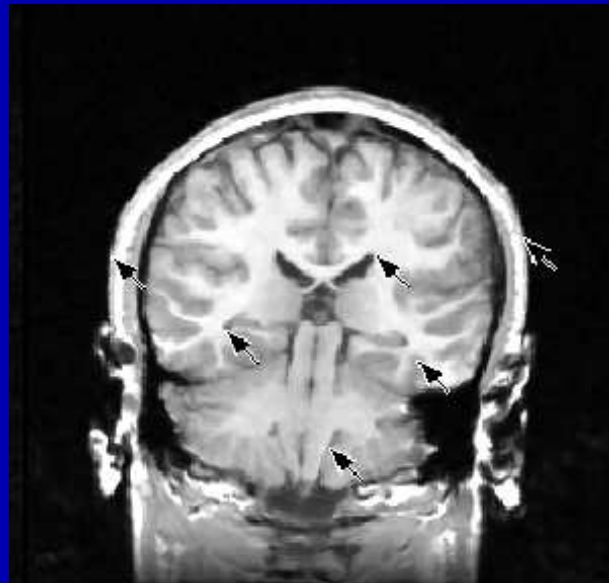
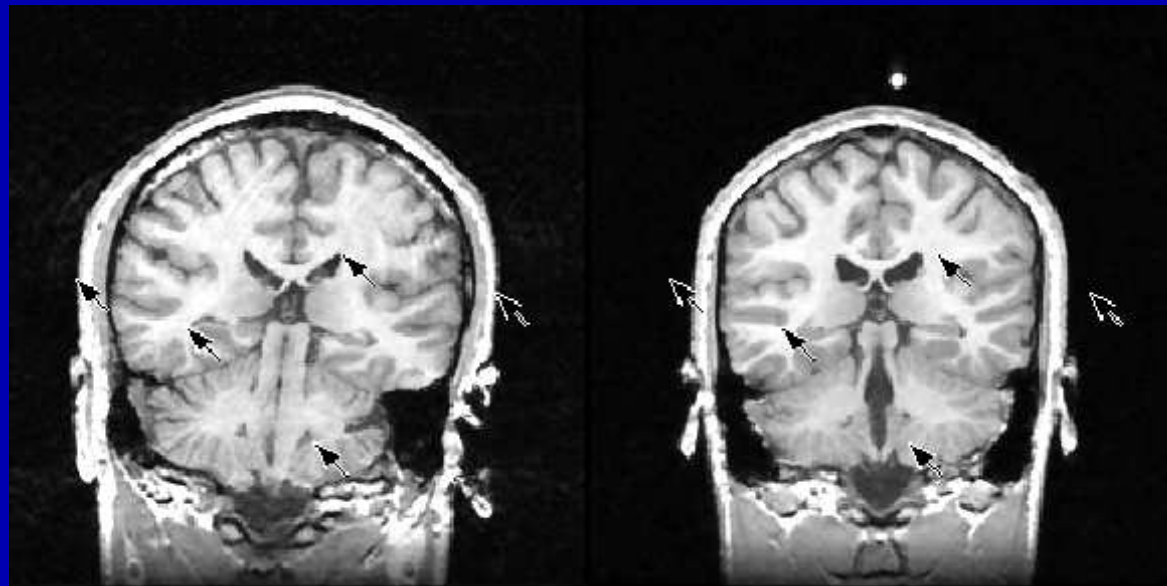


*3D reconstruction of the cortical surface and the ischemic area from rat's brain histological slices*

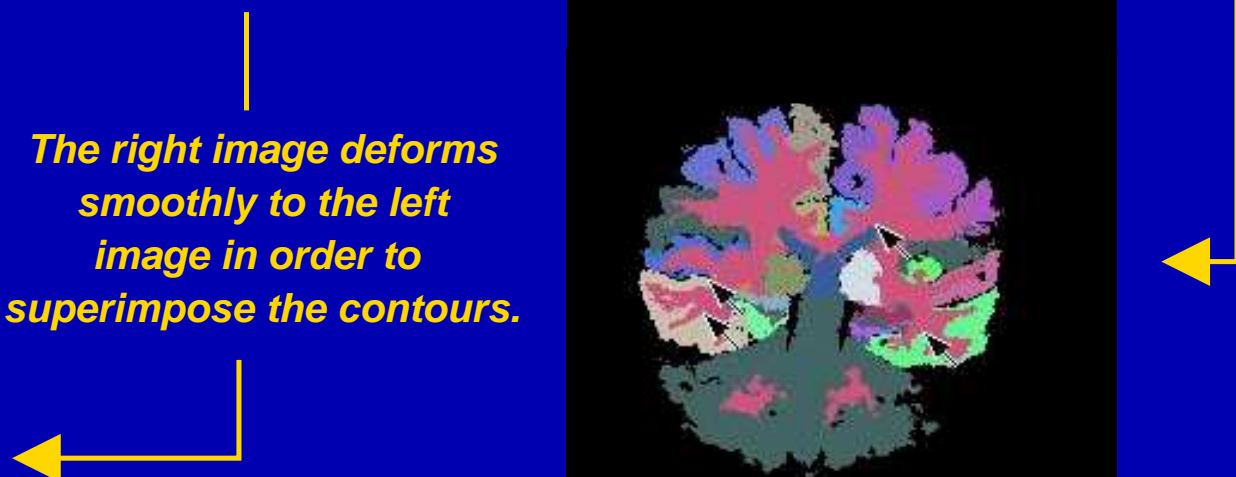
## 2. Registration of data



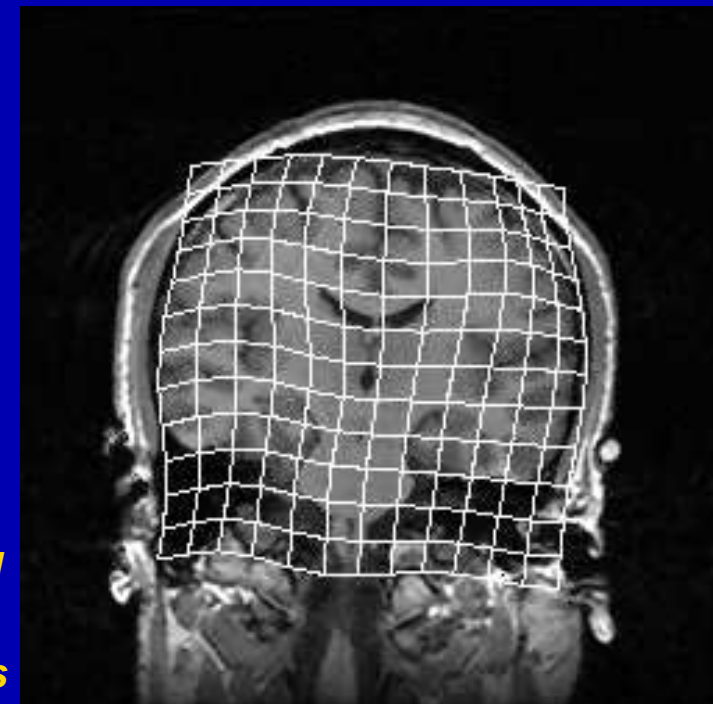
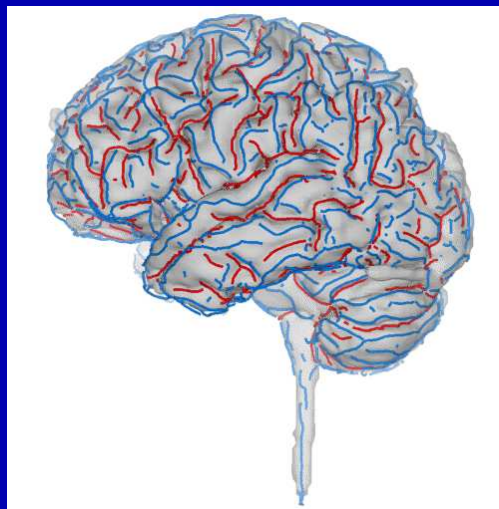
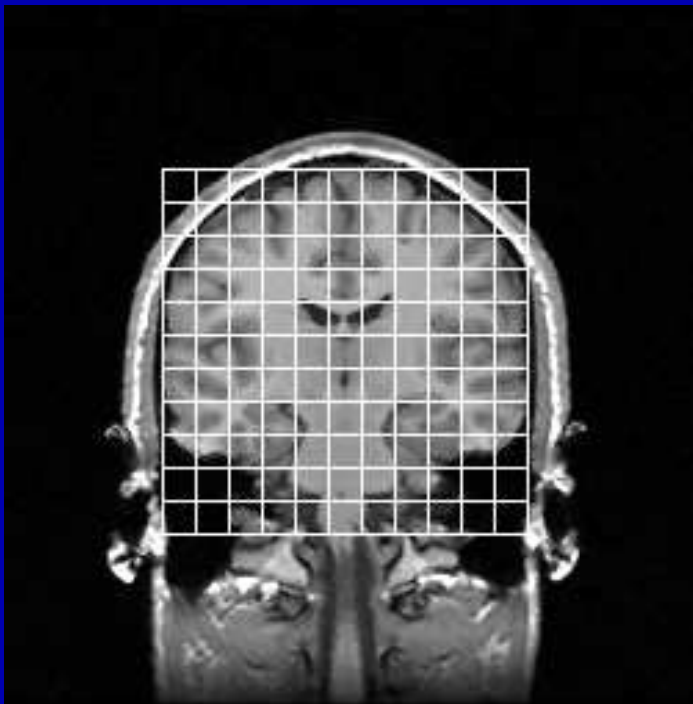
Different subject, same modality, same FOV



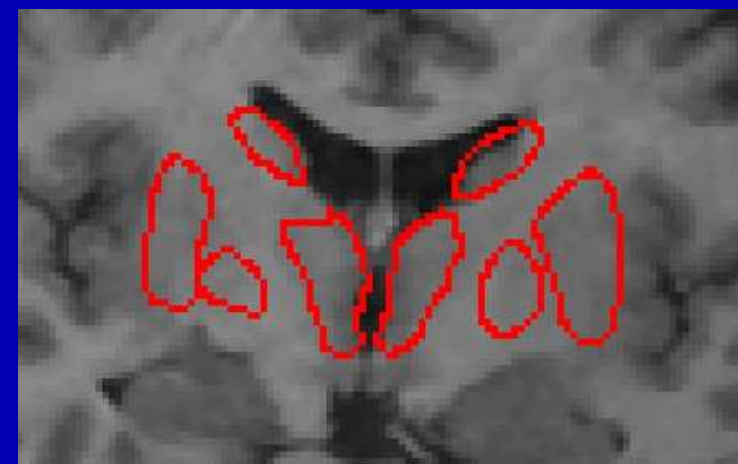
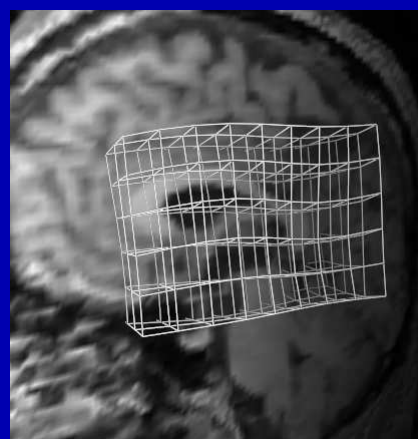
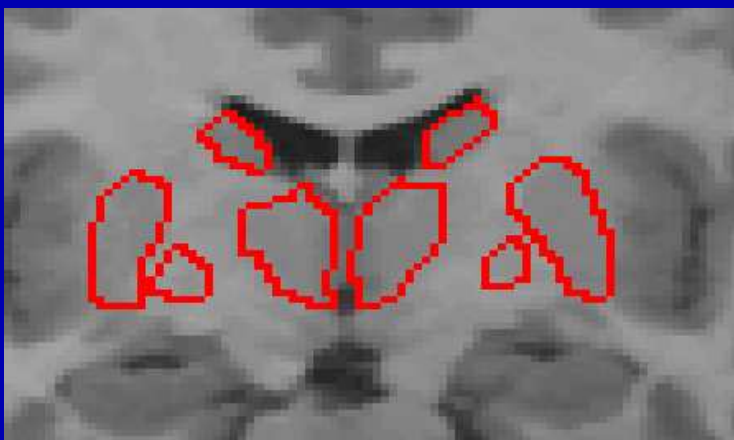
*The right image deforms smoothly to the left image in order to superimpose the contours.*



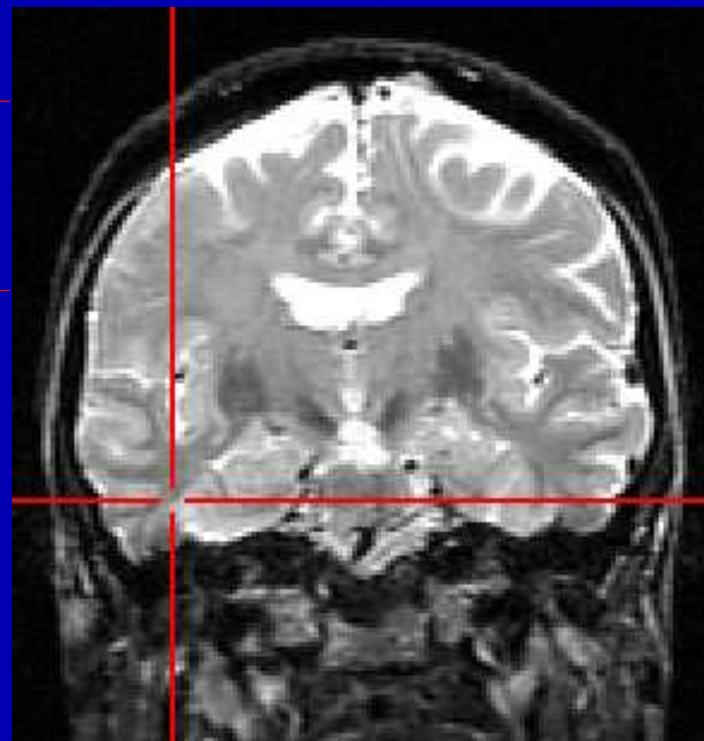
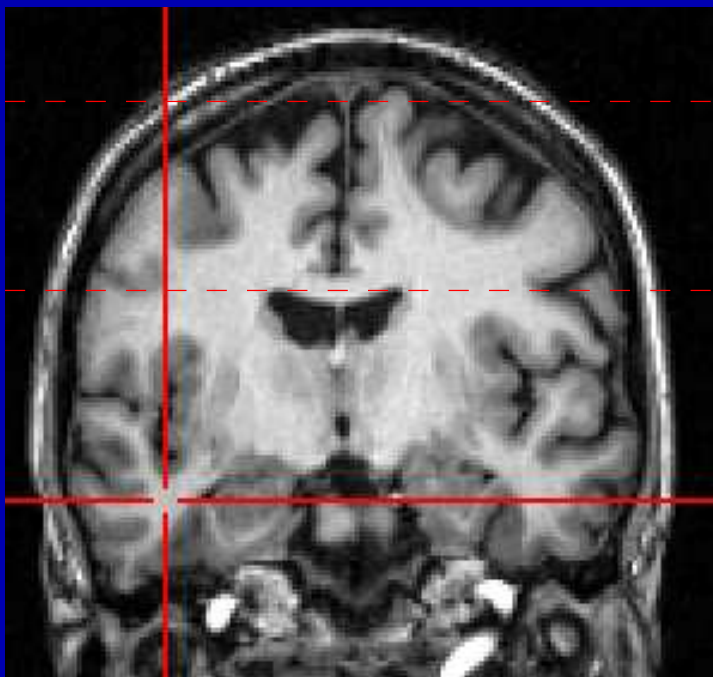
## Different subject, same modality, same FOV



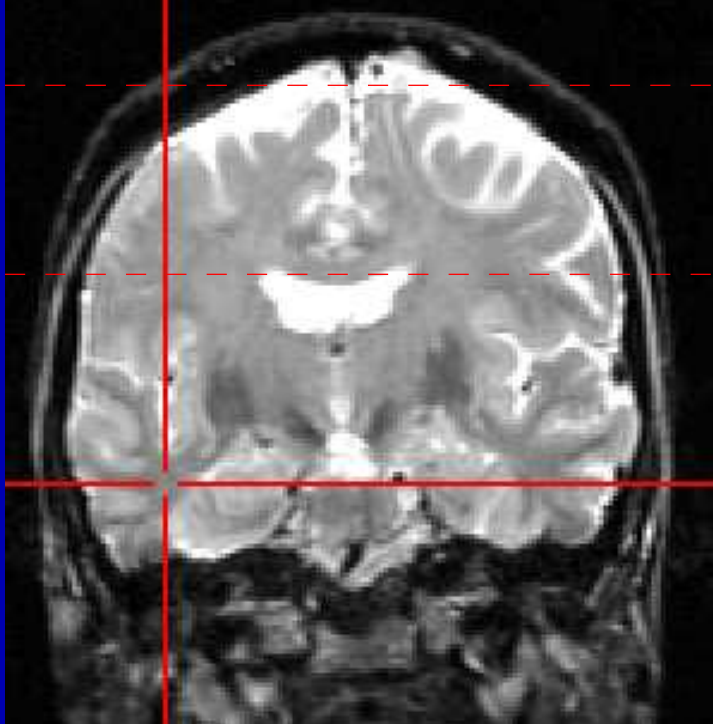
*The crest lines are extracted in the two images. They are matched and this defines a volume transformation.*



*Ste-T1*



Same subject  
Different modality  
Different FOV  
Artifacts



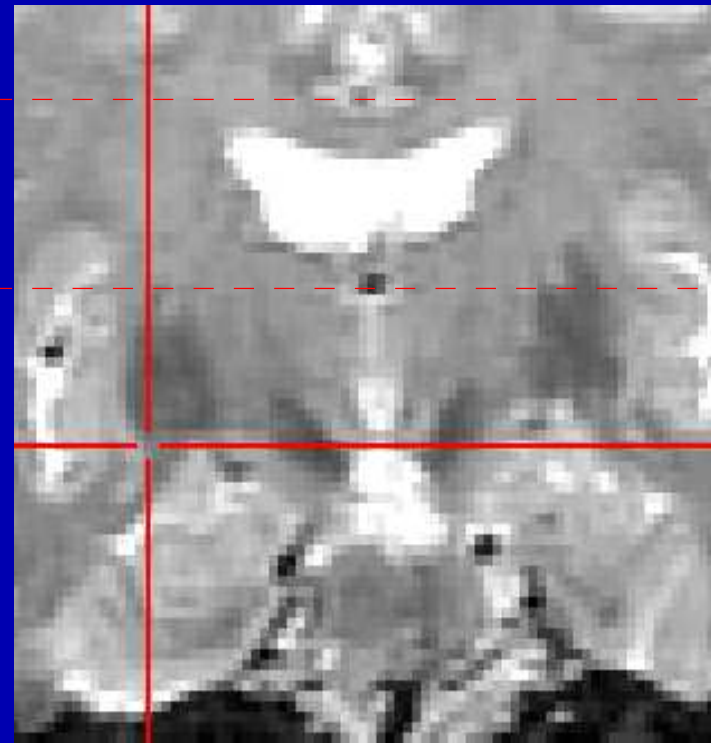
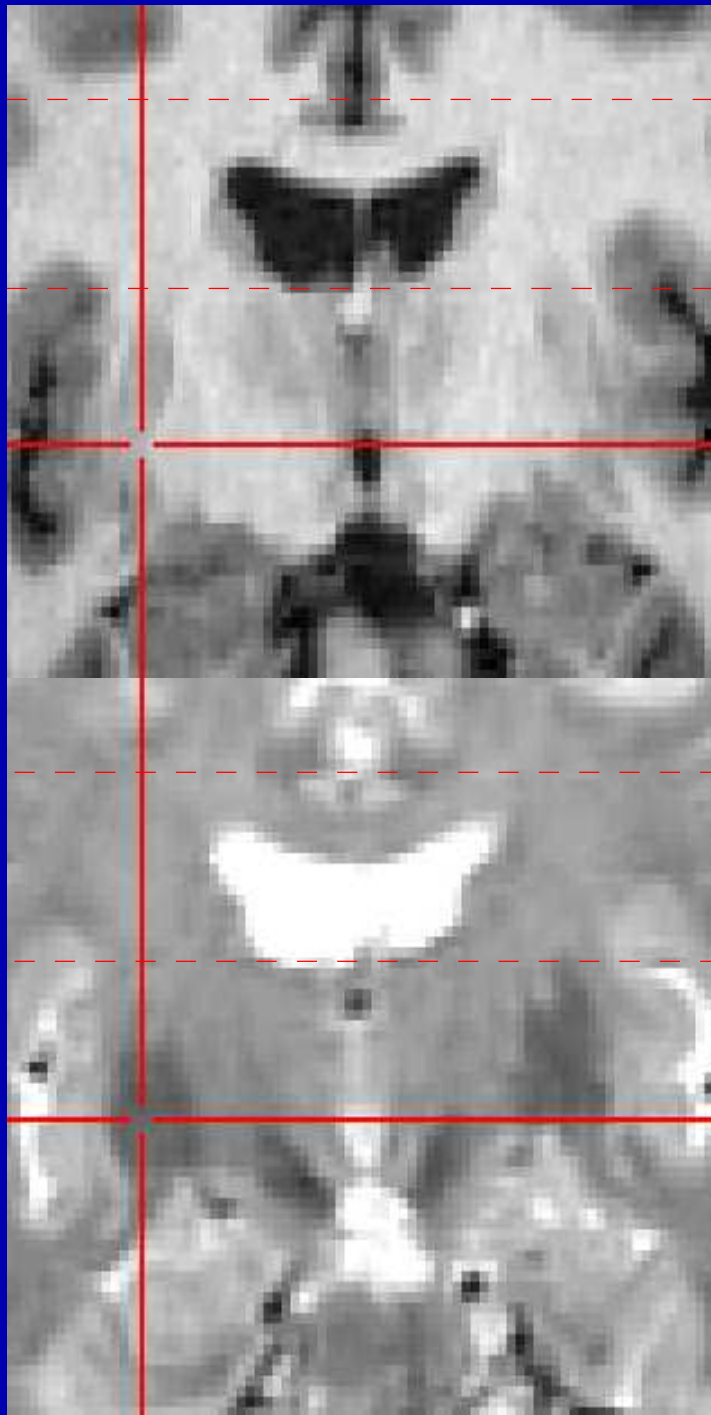
*High contrast T2*

A local similarity measure gives a local displacement vector at each voxel. Based on this vector field, a 3D transformation is computed.





*Ste-T1*



Same subject  
Different modality  
Different FOV  
Artifacts

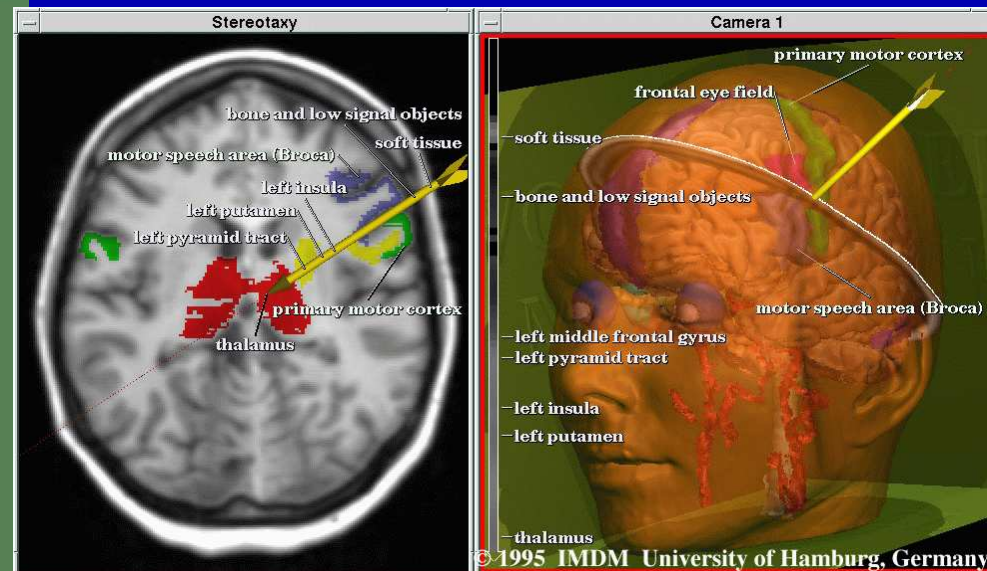
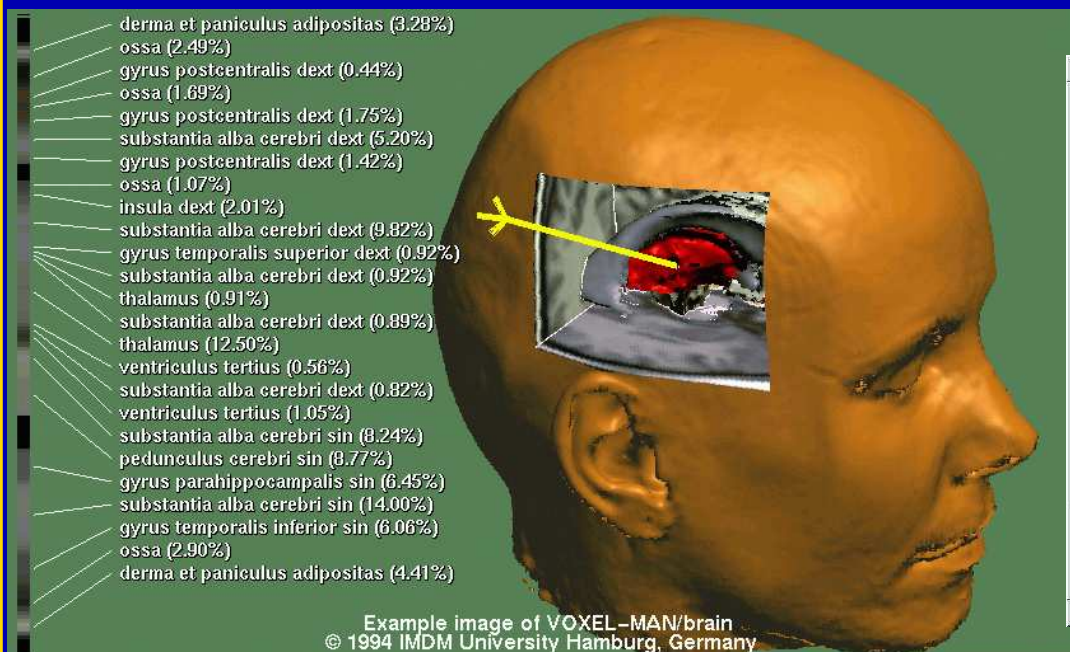
*High contrast T2*



## Assistance to the surgery

Once the stereotactic images has been labelled:

- ▶ find the optimal trajectory to the target
- ▶ avoid passage through critical structures



*Example of using a stereotaxy simulation  
on a reference patient (for teaching purpose)  
Voxel-Man, IMDM, University of Hamburg, Germany*

# Future Work

- **Construction of the 3D atlas**

**Now:** test and improvement of software  
collaboration on the elaboration of the acquisition procedure of histology data

**Soon:** test of software, in particular the reconstruction, on existing sections

- **Registration to ste-MR image**

**Now:** first result of registration between HR-T2 and ste-T1 MR images  
test of registration between atlas / T1 and ste-T1 images

**Soon:** extension to 3D of T2 / T1 registration algorithm  
quantitative study of the distortions