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100 years of living science

# 100

## Medical Imaging

– Part II, towards real-time interactive and functional imaging

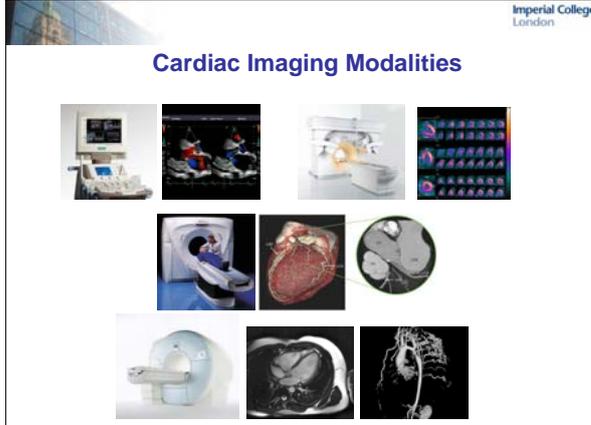


Professor Guang-Zhong Yang  
Institute of Biomedical Engineering & Department of Computing

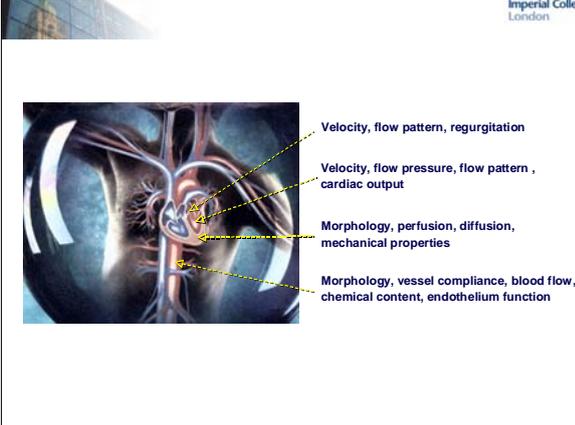
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## Cardiac Imaging Modalities

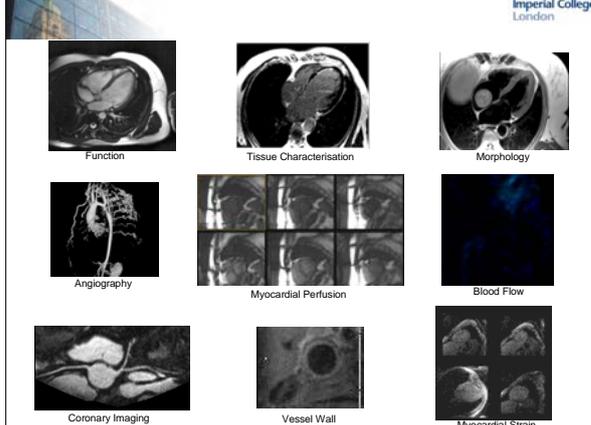


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- Velocity, flow pattern, regurgitation
- Velocity, flow pressure, flow pattern, cardiac output
- Morphology, perfusion, diffusion, mechanical properties
- Morphology, vessel compliance, blood flow, chemical content, endothelium function

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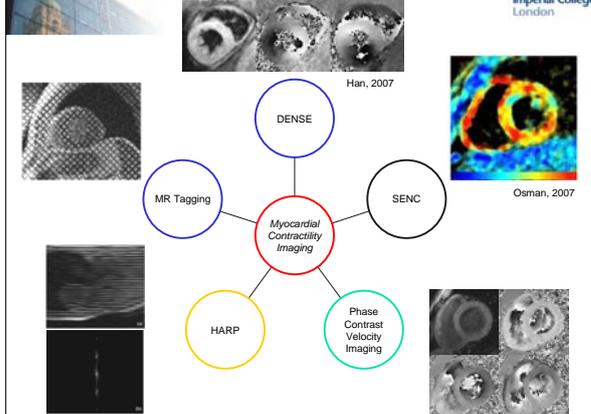
- Function
- Tissue Characterisation
- Morphology
- Angiography
- Myocardial Perfusion
- Blood Flow
- Coronary Imaging
- Vessel Wall
- Myocardial Strain

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## MRI Techniques for Myocardial Contractility

- MR tagging
- HARP - harmonic phase magnetic resonance imaging
- DENSE - displacement-encoded imaging with stimulated echoes
- Phase contrast myocardial velocity imaging

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MR Tagging

DENSE

SENC

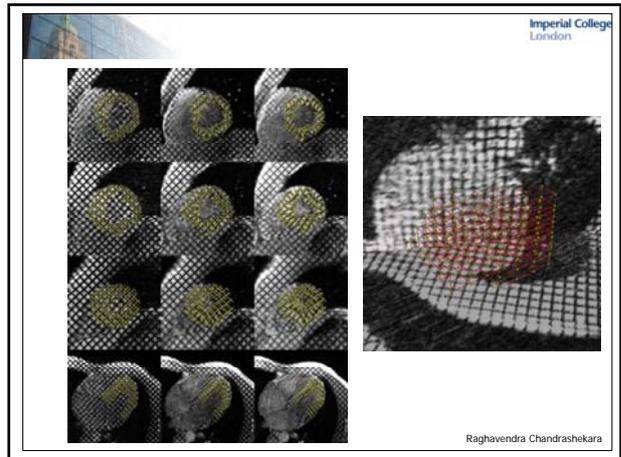
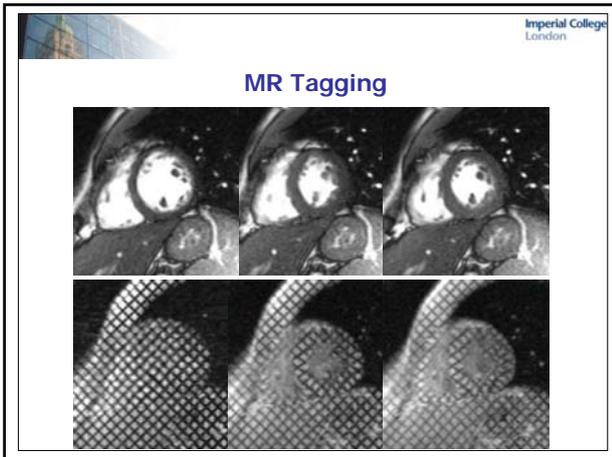
HARP

Phase Contrast Velocity Imaging

Myocardial Contractility Imaging

Han, 2007

Osman, 2007



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## Tagging Analysis Techniques

|                 |                   |           |                      |                  |
|-----------------|-------------------|-----------|----------------------|------------------|
| Amini et al     | radial+grid       | 2D ACM    | thin-plate splines   | motion simulator |
| Amini et al     | grid              | 3D ACM    | B-spline surfaces    | motion simulator |
| Young et al     | grid              | 3D ACM    | finite-element model | gel phantom      |
| Park et al      | grid              | 3D ACM    | deformable models    | none             |
| Kumar & Goldgof | grid              | 2D ACM    | thin-plate splines   | manual tracking  |
| Guttman et al   | radial & parallel | 2D ACM/TM | none                 | none             |

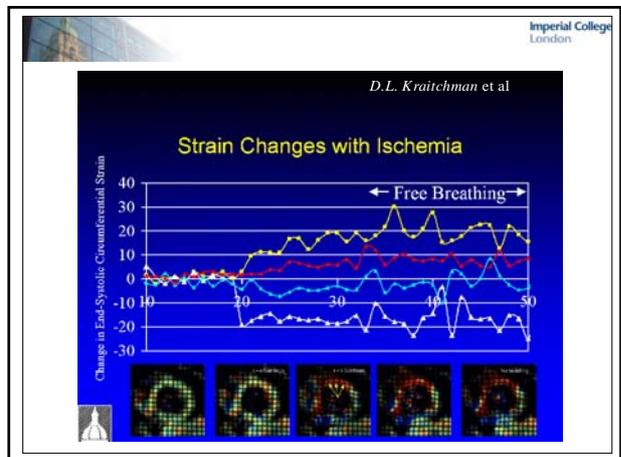
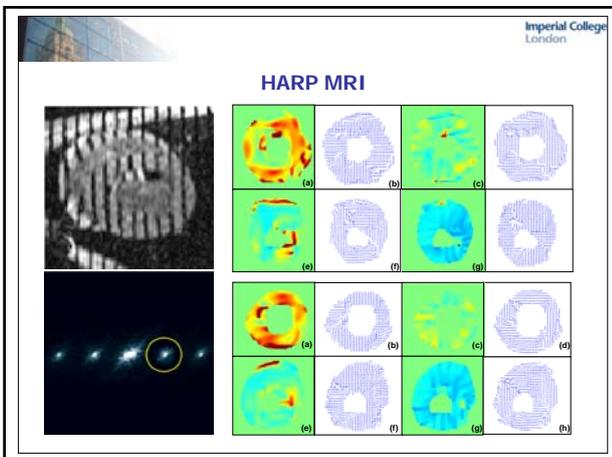
*Active contour models (ACM), template matching (TM), optical flow (OF), harmonic phase (HARP).*

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## Tagging Analysis Techniques

|                  |          |           |                             |                              |
|------------------|----------|-----------|-----------------------------|------------------------------|
| O'Dell et al     | parallel | 3D ACM/TM | series expansion            | motion simulator             |
| Declerck et al   | parallel | 3D ACM/TM | planispheric transformation | none                         |
| Denney & Prince  | parallel | 3D ACM/TM | Fisher estimation           | motion simulator             |
| Prince & McVeigh | grid     | 2D OF     | velocity fields             | motion simulator and phantom |
| Gupta & Prince   | grid     | 2D OF     | velocity fields             | motion simulator             |
| Dougherty et al  | grid     | 2D OF     | velocity fields             | gel phantom                  |
| Osman et al      | grid     | 2D        | - HARP                      | motion simulator             |

*Active contour models (ACM), template matching (TM), optical flow (OF), harmonic phase (HARP).*



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## DENSE

few ms ~ 1s  
90° T<sub>m</sub> 90° Image Acq

Initial phase maps      Phase shifts

Aletras, Ding, Balaban, and Wen, 1999

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## MR Velocity Imaging

- Moran, PR (Magn Reson Imaging, 1982) - theory of phase velocity imaging
- Redpath TW, et al. (Phys Med Biol, 1984) & Feinberg DA, et al. (Magn Reson Med, 1985) - first Fourier velocity imaging
- van Dijk, P (J Comput Assist Tomogr, 1984) & Bryant DJ, et al. (J Comput Assist Tomogr, 1984) - First Phase mapping velocity images

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Saturation washin enhancement, 1982, Hammersmith, London

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## Phase Contrast Velocity Mapping

Gradient Waveform

Magnetic Field

Signal Phase

Stationary Material      Flowing Material

Time 1      Time 2

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### Gradient Waveforms

Reference

+

-

Velocity encoded

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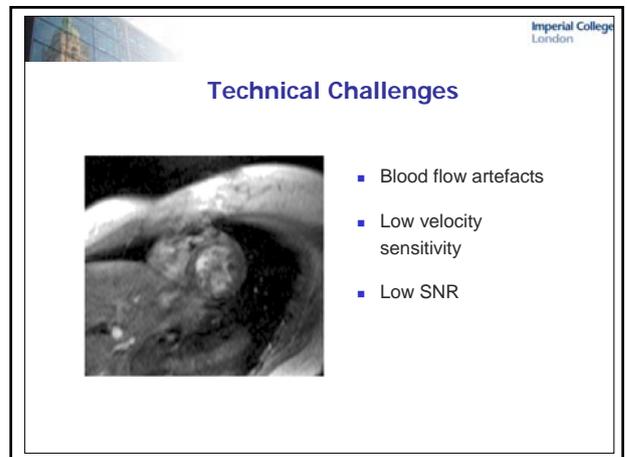
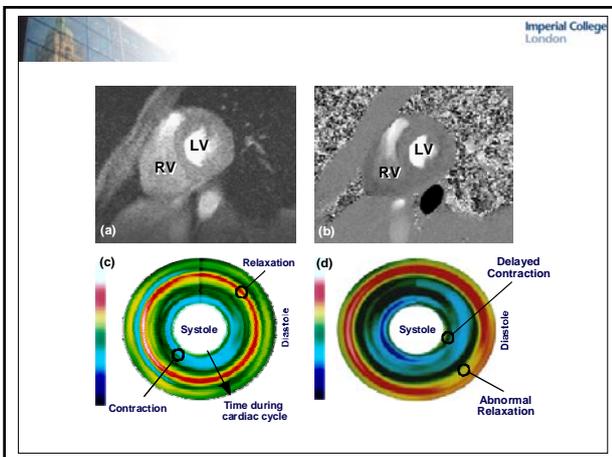
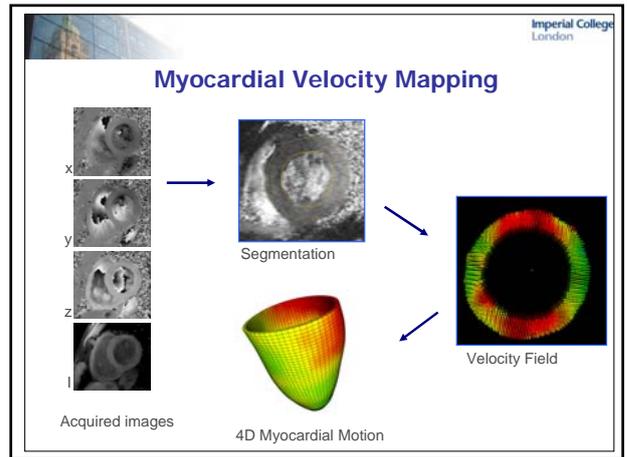
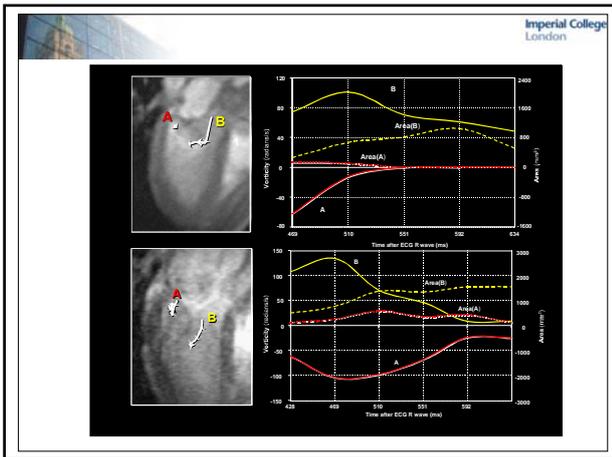
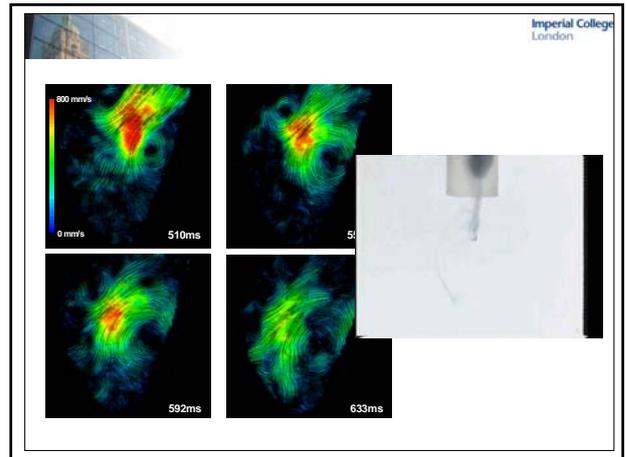
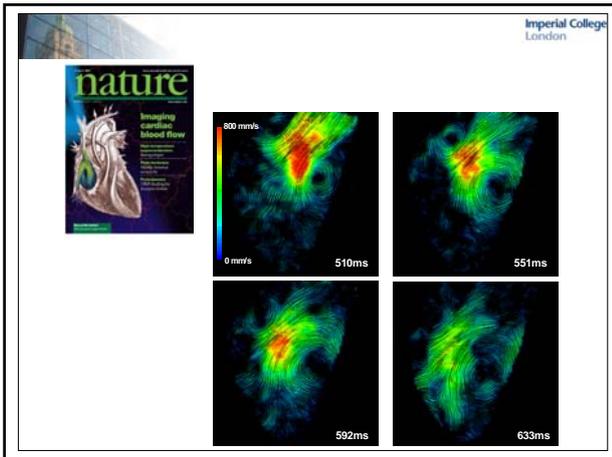
### Gradient Waveforms

Reference

+

-

Velocity encoded



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## Presaturation Slab

Reduces flow artefacts in the phase-encode direction

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## Computational Requirement

**Preprocessing**

- phase background correction
- phase unwrapping
- vector field restoration

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**Contractility and modelling**

- converting Eulerian velocity field to Lagrangian displacement (e.g. Fourier tracking, forward-backward integration)
- incorporating different regularization schemes (mainly geometrical, e.g. deformable mesh, spline models)
- incorporating biomechanical constraints (e.g., mass conservation, fibre-orientation) and the use of FEM

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## Computational Requirement

**Preprocessing**

- phase background correction
- phase unwrapping
- vector field restoration

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**Existing approaches**

- Horn and Schunk, 1981 (optical flow with Euler-Lagrange)
- Song et al, 1993 (Poisson equation)
- Yang et al, 1993 (POCS)
- Buonocore, 1994 (divergence minimisation)
- Herment et al, 1999 (spatial regularization with diffusion process)
- Fatouraee & Amini, 2003 (divergence free & stream function)
- Ng and Yang 2003, Carmo & Yang, 2004 (total variation restoration)

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## Computational Requirement

**Preprocessing**

- phase background correction
- phase unwrapping
- **vector field restoration**

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## Total Variation Vector Restoration

- Removes noise in the velocity vector field
- Formulated as a constrained optimization problem

$$\text{Min } E^{TV} = \sum_{\alpha} \left[ \sum_{\beta \in N_{\alpha}} d_{\beta}^2(u_{\beta}, u_{\alpha}) \right]^{\frac{1}{2}}$$

$$\text{Subject to } h(u) = \frac{1}{2} \left[ \sum_{\alpha} d_{\alpha}^2(u_{\alpha}, u_{\alpha}^0) - |\Omega| \sigma^2 \right] = 0$$

where  $d(f, g)$  is the embedded Euclidean distance between vectors  $f$  &  $g$   
 $\Omega$  is the image domain,  
 $\sigma^2$  is the variance of the noise of the image,  
 $u$  is the original image to be restored and,  
 $u^0$  is the noisy image

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## Total Variation Vector Restoration

**Lagrangian function:**

$$L(u, \lambda) = \sum_{\alpha} \left[ \sum_{\beta \in N_{\alpha}} d_{\beta}^2(u_{\beta}, u_{\alpha}) \right]^{\frac{1}{2}} + \frac{\lambda}{2} \left[ \sum_{\alpha} d_{\alpha}^2(u_{\alpha}, u_{\alpha}^0) - |\Omega| \sigma^2 \right]$$

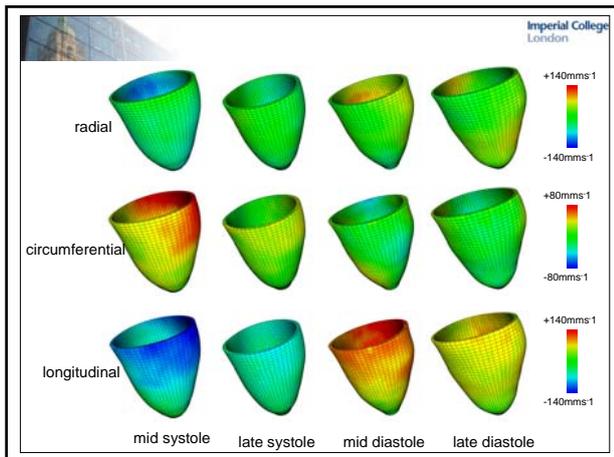
**First order Lagrangian method:**

$$u_{\alpha}^{n+1} = u_{\alpha}^n + \Delta t \cdot \prod_{\beta \in N_{\alpha}} \left[ \sum_{\beta \in N_{\alpha}} w_{\beta}^{\alpha} u_{\beta} + \mathcal{L}^{\alpha} u_{\alpha}^n \right]$$

$$\mathcal{L}^{\alpha} = \mathcal{L} + \Delta t \cdot \frac{\lambda}{2} \left[ \sum_{\alpha} d_{\alpha}^2(u_{\alpha}, u_{\alpha}^0) - |\Omega| \sigma^2 \right]$$

where

$$w_{\beta}^{\alpha} = \left( \frac{1}{e(u, \alpha)} + \frac{1}{e(u, \beta)} \right)$$



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### Computational Requirement

**Preprocessing**

- phase background correction
- phase unwrapping
- **vector field restoration**

**Contractility and modelling**

- **converting Eulerian velocity field to Lagrangian displacement (e.g. Fourier tracking, forward-backward integration)**
- **incorporating different regularization schemes (mainly geometrical, e.g. deformable mesh, spline models)**
- **incorporating biomechanical constraints (e.g., mass conservation, fibre-orientation) and the use of FEM**

early-systole late-systole  
early-diastole late-diastole

Detailed description: This slide outlines the computational requirements for cardiac motion analysis. It is divided into 'Preprocessing' and 'Contractility and modelling'. Preprocessing includes phase background correction, phase unwrapping, and vector field restoration. Contractility and modelling involves converting Eulerian velocity fields to Lagrangian displacements using techniques like Fourier tracking or forward-backward integration, incorporating various regularization schemes (geometrical, deformable mesh, spline models), and adding biomechanical constraints such as mass conservation and fibre orientation, often using Finite Element Method (FEM). Small images show the LV at early and late systole and diastole.

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### Computational Requirement

**Contractility and modelling**

- converting Eulerian velocity field to Lagrangian displacement (e.g. Fourier tracking, forward-backward integration)
- incorporating different regularization schemes (mainly geometrical, e.g. deformable mesh, spline models)
- incorporating biomechanical constraints (e.g., mass conservation, fibre-orientation) and the use of FEM

**Existing approaches**

- Young and Axel, 1992-1995 (model based approach and FEM)
- Van Wedeen, 1992 (strain rate tensor)
- Zhu, 1996, 1997, 1999 (Fourier tracking and spatio-temporal model)
- Meyer et al, 1996 (stochastic approach)
- Park et al, 1996 (volumetric deformable models)
- Amini et al, 1998 (coupled b-snake grids and constrained thin-plate splines)
- Arai et al 1999 (global local decoupled analysis)
- Masood et al 2002 (spline based virtual tagging)
- Chandrashekhara and Rueckert, 2004 (spline based free form registration)
- Lee et al 2006, 2007 (FEM, Kriging and TV)

Detailed description: This slide provides a list of existing approaches for cardiac motion analysis. It includes references to works by Young and Axel (1992-1995), Van Wedeen (1992), Zhu (1996, 1997, 1999), Meyer et al (1996), Park et al (1996), Amini et al (1998), Arai et al (1999), Masood et al (2002), Chandrashekhara and Rueckert (2004), and Lee et al (2006, 2007). The methods mentioned include model-based approaches, strain rate tensor analysis, Fourier tracking, stochastic approaches, volumetric deformable models, b-snake grids, spline-based virtual tagging, and free form registration.

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Lagrangian regularization (thin plate, Navier splines)

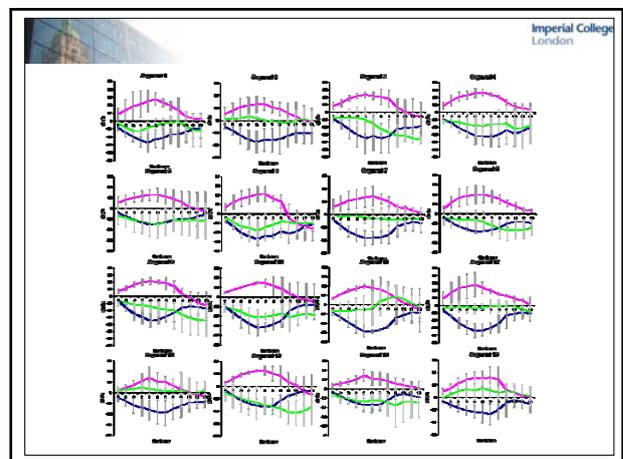
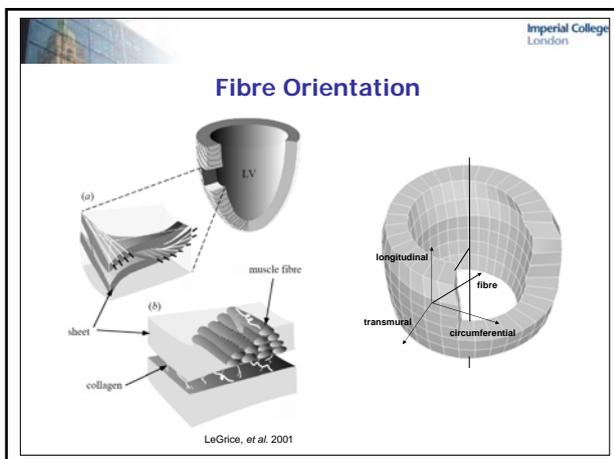
Statistical and spatio-temporal models

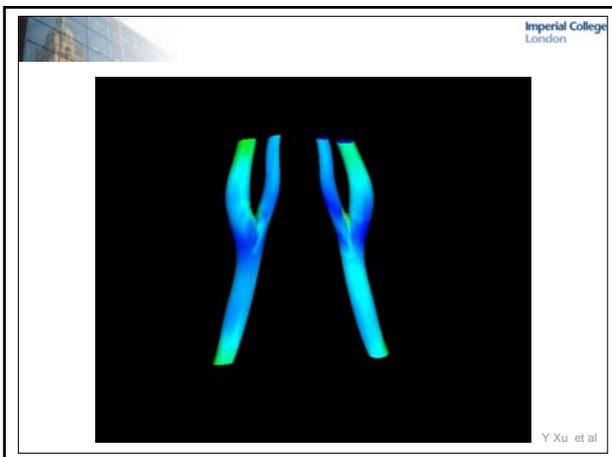
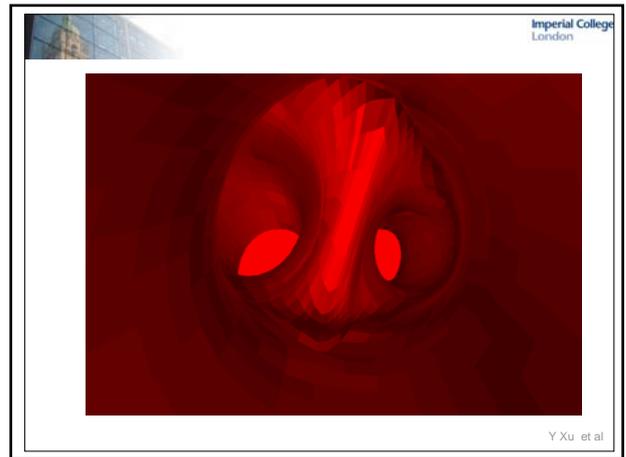
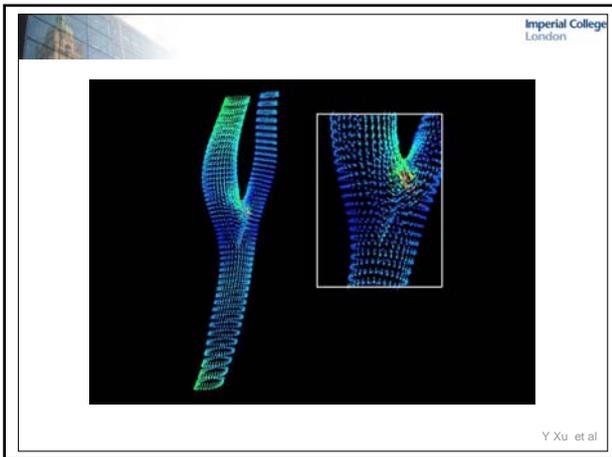
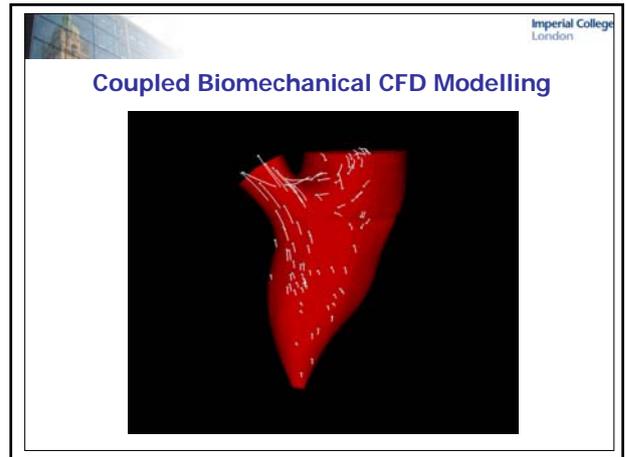
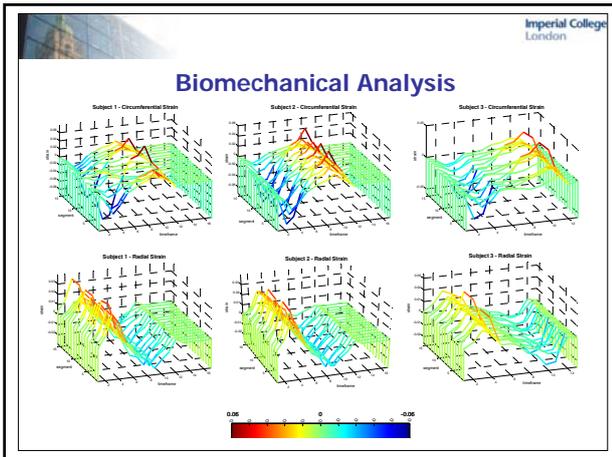
Physical based modelling (incorporating material property, anisotropic fibre orientation, and intra-ventricular pressure)

Semi-physical based modelling (e.g. virtual tagging incorporating mass conservation and the use of Kriging)

Coupled biomechanical and CFD modelling

Detailed description: This slide illustrates different modelling approaches for cardiac motion analysis. It shows two LV models: one with a thin plate and one with a more complex structure. The approaches are categorized into Lagrangian regularization (thin plate, Navier splines), Statistical and spatio-temporal models, Physical based modelling (incorporating material property, anisotropic fibre orientation, and intra-ventricular pressure), Semi-physical based modelling (e.g. virtual tagging incorporating mass conservation and the use of Kriging), and Coupled biomechanical and CFD modelling.

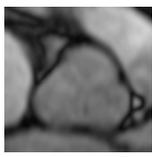




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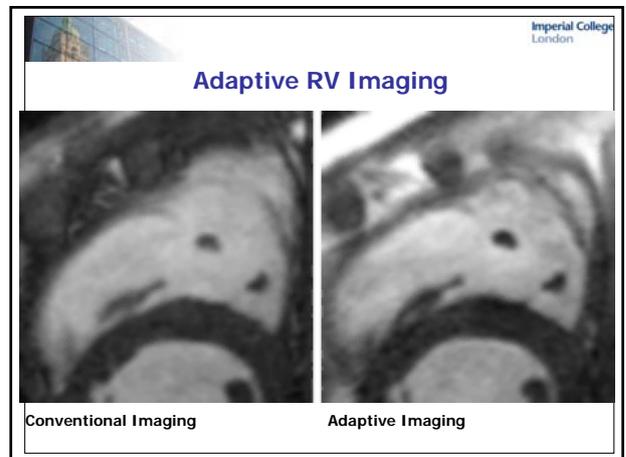
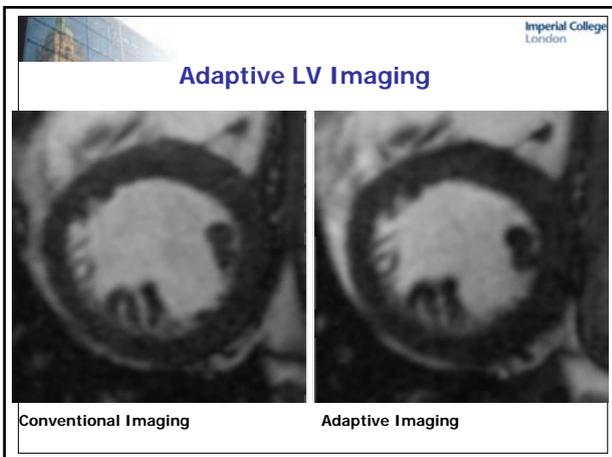
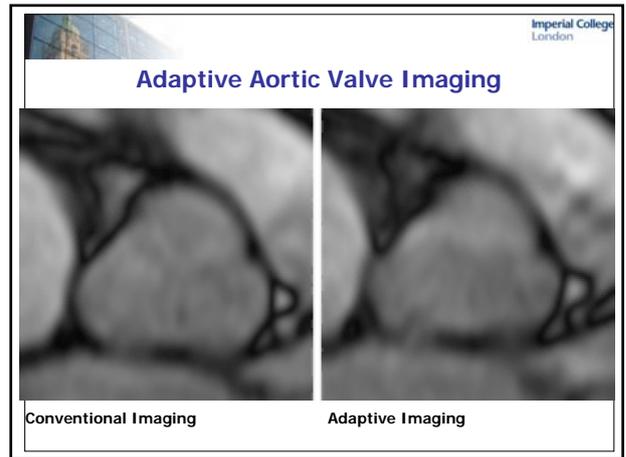
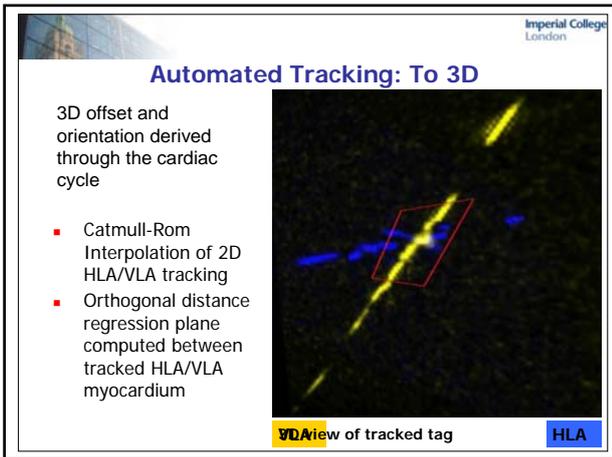
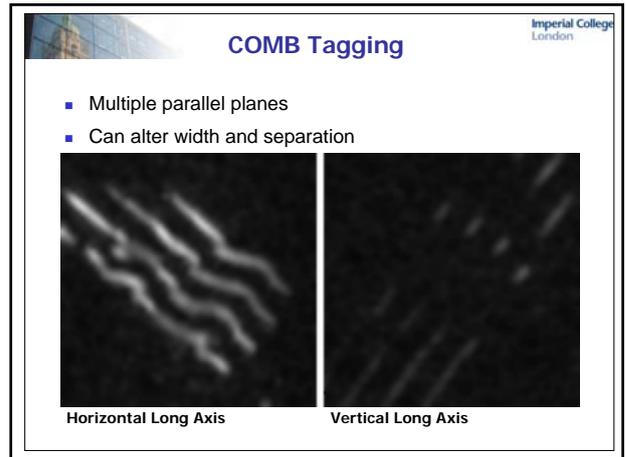
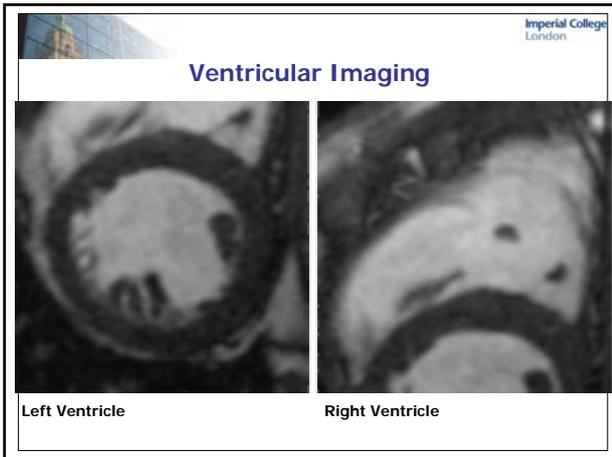
### Valve Imaging

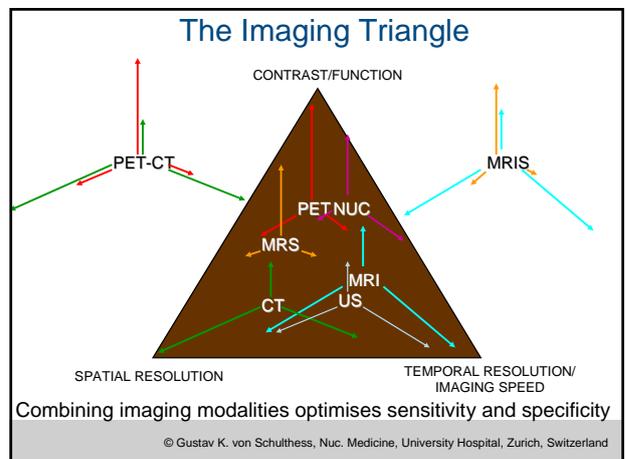
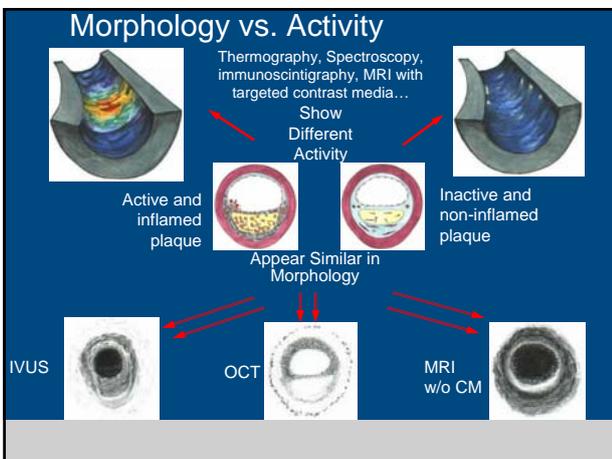
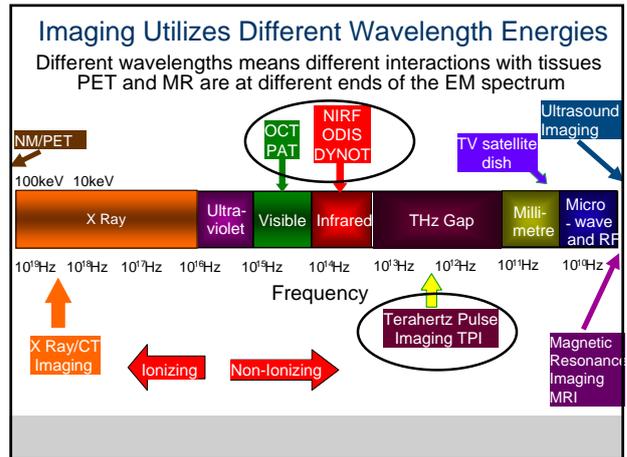
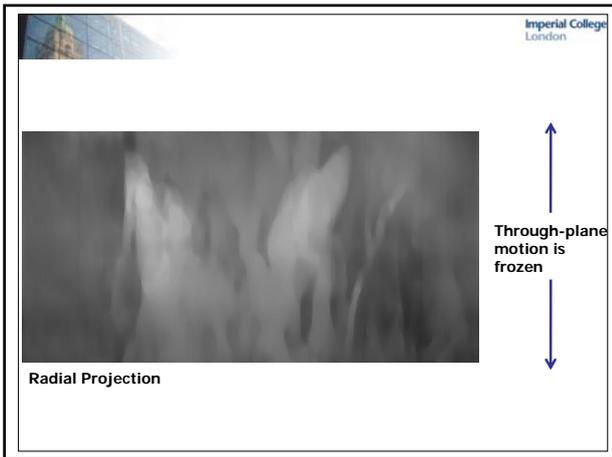
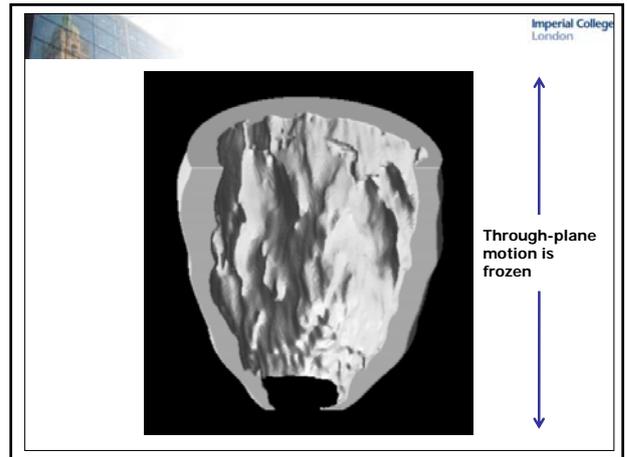
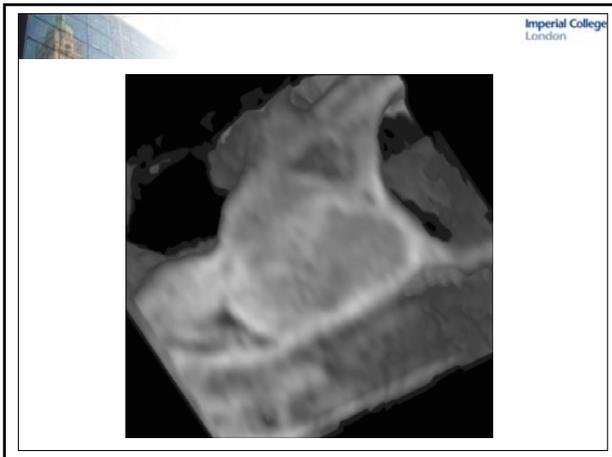
- Difficulty capturing valve leaflets
- Diastolic motion leads to underestimation of regurgitation\*
- Ultrasound currently preferred




(a) End Systole    (b) End Systole    (a) End Diastole    (b) End Diastole

\* Kozerke *et al.*, *J. Magn. Reson. Imaging*, 14 (2001), 106-112



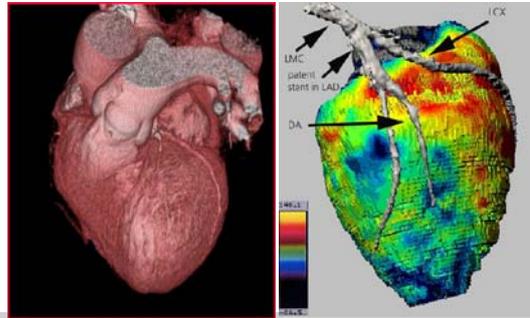


### PET/CT Cardiovascular Fusion



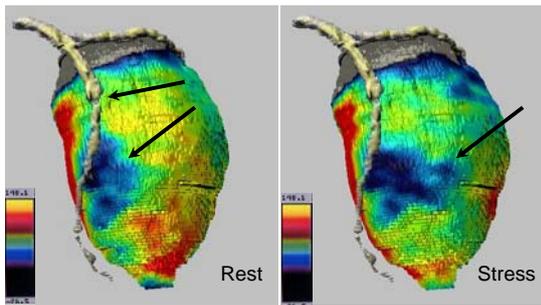
Courtesy of U Zurich, Switzerland

### PET/CT Cardiovascular Fusion



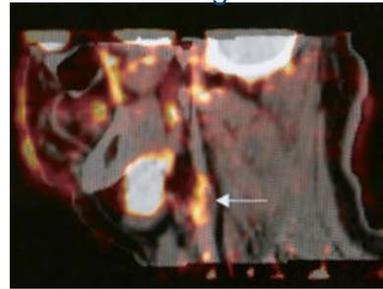
Courtesy of University Hospital Zurich, Switzerland

### PET/CT Cardiovascular Fusion



Courtesy of University Hospital Zurich, Switzerland

### Uptake of $^{18}\text{F}$ -FDG in Symptomatic Plaque PET/CT Image Fusion



Uptake of  $^{18}\text{F}$ -FDG is higher in inflamed carotid artery plaque and could be an indicator for plaque rupture

Rudd et al Cambridge University

### MR Guided HI FUS

### Guided Ultrasound Therapy

Encapsulated Drugs Released by Ultrasound at Disease Site

Ultrasound Hyperthermia

Destroy or Treat Disease Tissue

